

Ultra-deformable lipid vesicles localise Amphotericin B in the dermis for the treatment of skin infectious diseases

Raquel Fernández-García^{1#}, Larry Statts^{2#}, Jéssica A. de Jesus³, Maria Auxiliadora Dea-Ayuela⁴, Liliana Bautista², Rúben Simão¹, Francisco Bolás-Fernández⁵, Maria Paloma Ballesteros^{1,6}, Marcia Dalastra Laurenti³, Luiz F. D. Passero^{7,8}, Aikaterini Lalatsa^{2*}, Dolores R. Serrano^{1,6*}.

¹Departamento de Farmacia Galénica y Tecnología Alimentaria, Facultad de Farmacia, Universidad Complutense de Madrid. Plaza Ramón y Cajal s/n, 28040, Madrid (Spain)

²Biomaterials, Bio-engineering and Nanomedicines (BioN) laboratory, Institute of Biomedical and Biomolecular Sciences, School of Pharmacy and Pharmaceutical Sciences, University of Portsmouth, St. Michael's Building, White Swan Road, Portsmouth (United Kingdom)

³Laboratory of Pathology of Infectious Diseases (LIM-50), Medical School, University of São Paulo, Avenida Dr. Arnaldo 455, 01246903 Cerqueira César, SP (Brazil)

⁴Departamento de Farmacia. Facultad de Ciencias de la Salud. Universidad CEU Cardenal Herrera. Carrer Santiago Ramón y Cajal, s/n. 46113 Valencia (Spain)

⁵Departamento de Microbiología y Parasitología, Facultad de Farmacia, Universidad Complutense de Madrid. Plaza Ramón y Cajal s/n, 28040, Madrid (Spain)

⁶Instituto Universitario de Farmacia Industrial, Facultad de Farmacia, Universidad Complutense de Madrid. Plaza Ramón y Cajal s/n, 28040, Madrid (Spain)

⁷São Paulo State University (UNESP), Institute of Biosciences, São Vicente. Praça Infante Dom Henrique, s/n, 11330-900 São Vicente, SP, (Brazil)

⁸São Paulo State University (UNESP), Institute for Advanced Studies of Ocean, São Vicente. Av. João Francisco Bendorp, 1178, 11350-011 São Vicente, SP (Brazil)

First co-authorship shared

*Corresponding authors:

Dr Aikaterini Lalatsa
School of Pharmacy and Biomedical Sciences
University of Portsmouth
White Swan Road,
Portsmouth, PO1 2DT
Email: katerina.lalatsa@port.ac.uk
Tel: +44 2392 84 3929

Dolores R. Serrano
Departamento de Farmacia Galénica y Tecnología Alimentaria
Facultad de Farmacia
Universidad Complutense de Madrid
28040-Madrid, Spain
Email: drserran@ucm.es
Tel: +34 91 394 1620

ABSTRACT

Cutaneous fungal and parasitic diseases remain challenging to treat, as available therapies are unable to permeate the skin barrier. Thus, treatment options rely on systemic therapy, which fail to produce high drug local concentrations but can lead to significant systemic toxicity. Amphotericin B (AmB) is highly efficacious in the treatment of both fungal and parasitic diseases such as cutaneous leishmaniasis, but is only reserved for parenteral administration in patients with severe pathophysiology. Here, we have designed and optimised AmB-transfersomes [93.5 % encapsulation efficiency, size of 150 nm, and good colloidal stability (-35.02 mV)] that can remain physicochemically stable (>90 % drug content) at room temperature and 4 °C over 6 months when lyophilised and stored under desiccated conditions. AmB-transfersomes possessed good permeability across mouse skin ($4.91 \pm 0.41 \mu\text{g}/\text{cm}^2/\text{h}$) and 10-fold higher permeability across synthetic Strat-M[®] membranes. *In vivo* studies after a single topical application in mice showed permeability and accumulation within the dermis (>25 μg AmB /g skin at 6 h post-administration) indicating the delivery of therapeutic amounts of AmB for mycoses and cutaneous leishmaniasis, while a single daily administration in *Leishmania (Leishmania) amazonensis* infected mice over 10 days resulted in excellent efficacy (98 % reduction in *Leishmania* parasites). Combining the application of AmB-transfersomes with metallic microneedles *in vivo* increased levels in the SC and dermis but is unlikely to elicit transdermal levels. In conclusion, AmB-transfersomes are promising and stable topical nanomedicines that can be readily translated for parasitic and fungal infectious diseases.

KEYWORDS

Amphotericin B, transfersomes, ultra-deformable lipid vesicles, fungal infections, leishmaniasis, tape stripping

1
2
3 Skin infections are a common public health problem in developed and developing countries. However,
4 they remain challenging to treat as available therapies are unable to permeate the skin barrier and
5 localise the drug within the skin at high concentration without the need of frequent administrations or
6
7 in some severe infections such as cutaneous and mucocutaneous leishmaniasis of prolonged
8 intralesional administration. Thus, these patients rely on systemic therapy (oral or intravenous) that fails
9 to result in high local concentration in the skin, while able to lead to significant systemic toxicity.
10
11

12
13 Amphotericin B (AmB) is a macrolide chemotherapeutic produced by *Streptomyces nodosus*¹ that has
14 been the “gold-standard” of the antifungal therapy since its commercialisation, while remaining the first
15 line therapy in the developed world for the treatment of leishmaniasis². Although highly effective with
16 limited occurrence of resistance, AmB is a large, amphiphilic, poorly water-soluble drug (below 0.001
17 mg/ml) with poor permeability across biological barriers^{1, 3}. AmB is currently only licensed as a
18 liposomal formulation for parenteral administration (AmBisome[®]) as older micellar formulations are
19 highly nephrotoxic. AmBisome[®] apart from being highly expensive and thus not really an option for
20 the treatment of neglected parasitic diseases such as cutaneous and mucocutaneous leishmaniasis is also
21 highly unstable at room temperature⁴. A cream containing 3 % of AmB (Anfoleish) for topical use is
22 currently under clinical trials (NCT01845727), but preliminary results have shown variable efficacy in
23 patients with cutaneous leishmaniasis which can be the result of a limited permeability across the skin
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

Ultra-deformable lipid vesicles, also known as transferosomes or transfersomes (TFs), are drug delivery systems with shown potential to overcome the stratum corneum and reach deeper regions of the skin promoting drug targeting, while minimizing adverse effects⁷⁻⁹. TFs consist of lipids, an edge activator and a small amount of ethanol (<10 %) ⁸ forming ultradeformable vesicles that permeate the skin following the natural water osmotic gradient¹⁰. Previous reports to develop AmB-TFs demonstrated their capability *in vitro* but *in vivo* proof of concept has not been shown¹¹. The hypothesis underpinning this work is that the encapsulation of AmB within TFs can enable the AmB permeation across the skin and localise it in the epidermis and dermis in effective concentrations for the treatment of fungal and parasitic infections in a stable formulation for topical application. In this respect, we optimised AmB-TFs using quality by design (QbD) to ensure high entrapment efficiency, small size and colloidal stability and assess their stability at room temperature and under refrigeration after prepared formulations were lyophilised and stored under desiccated conditions. To understand their permeation across the skin and drug localisation, we undertook *ex vivo* Franz cell diffusion assays across mouse skin and *in vivo* tape stripping experiments in mice. The efficacy of the formulation was demonstrated in *Candida albicans*, *C glabrata* and *C. parapsilosis* disk diffusion assays and *in vitro* efficacy against *Leishmania (Leishmania) amazonensis* and *Leishmania (Viannia) braziliensis* promastigotes and amastigotes, while their *in vivo* activity was also demonstrated in *L. (L.) amazonensis* infected mice

1
2
3 treated with AmB-TFs. Finally, *in vitro* toxicity in murine macrophages, haemolysis and histopathology
4 studies were performed to demonstrate the safety of the proposed transcutaneous formulation.
5
6

7 RESULTS

8 Design of experiments (DOE) studies and optimisation of AmB-TFs

9
10 The 17 experimental runs including independent and dependent variables are shown in table 1.
11
12

13 **Table 1. Independent variables and responses of all tested formulations.**
14

| Run | Independent variables | | | Dependent variables | | |
|-----|--------------------------|---------------------|-----------------------|---------------------|---------------------|---------------------------|
| | Amount of surfactant (%) | Amount of drug (mg) | Amount of ethanol (%) | Particle size (nm) | Zeta potential (mV) | Entrapment efficiency (%) |
| 1 | 6 | 1.25 | 8.5 | 107.8 | -25.11 | 66.62 |
| 2 | 6 | 1.25 | 0 | 190.3 | -27.96 | 82.08 |
| 3 | 13 | 2 | 0 | 806 | -36.74 | 67.46 |
| 4 | 13 | 0.5 | 8.5 | 823 | -31.98 | 77.52 |
| 5 | 13 | 1.25 | 4 | - | -49.76 | 91.1 |
| 6 | 13 | 1.25 | 4 | 145.7 | -29.95 | 80.1 |
| 7 | 6 | 0.5 | 4 | 118.2 | -27.67 | 69.59 |
| 8 | 20 | 2 | 4 | 363 | -20.68 | 42.55 |
| 9 | 13 | 1.25 | 4 | 88.2 | -34 | 82.16 |
| 10 | 13 | 0.5 | 0 | 204 | -34.03 | 94.63 |
| 11 | 20 | 1.25 | 8.5 | 351 | -33.78 | 77.4 |
| 12 | 13 | 2 | 8.5 | 556 | -30.93 | 56.87 |
| 13 | 20 | 0.5 | 4 | 1314 | -33.63 | 32.68 |
| 14 | 20 | 1.25 | 0 | 92.2 | -35.82 | 56.5 |
| 15 | 13 | 1.25 | 4 | 99.2 | -31.25 | 95.06 |
| 16 | 13 | 1.25 | 4 | 138.1 | -33.63 | 78.45 |
| 17 | 6 | 2 | 4 | 1091 | -20.16 | 44.9 |

15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

Polynomial analysis was carried out by a multilinear regression analysis method suggesting that the quadratic model was the best fit for particle size and entrapment efficiency (EE). The coefficients of the model equations generated for each critical quality attribute (Eq. 1 & 2 in S1.1 in SI) revealed goodness of fit (Fig. S1 in SI) of the experimental data to the selected model with high values of R^2 (0.9772 and 0.898 respectively) and low p-values < 0.05 (Table S1 in SI). None of the three factors evaluated showed a significant impact on the zeta potential and possessed a zeta potential lower than -20 mV (Table 1). Thus, zeta potential was not utilised to inform the optimisation of the AmB-TFs. The multilinear regression models for particle size and EE are described in supplementary material.

The amount of AmB and sodium deoxycholate have a positive effect on particle size (Fig. 1a-c, Fig. S2-S4 in SI). The greater the amount, the larger the particle size of the TFs. The lowest particle size was achieved with low-intermediate amounts of sodium deoxycholate (6-12 %) and a drug content below 1.8 mg per batch (Fig. S2 and S3 in SI).

In terms of EE, intermediate amounts of edge activator and AmB resulted in the greatest EE. The effect of the ethanol was not as sharply defined as a larger EE was obtained when using either a low or a high percentage (< 2% or > 7%) (Fig. 1d-f, Fig. S5-S7 in SI).

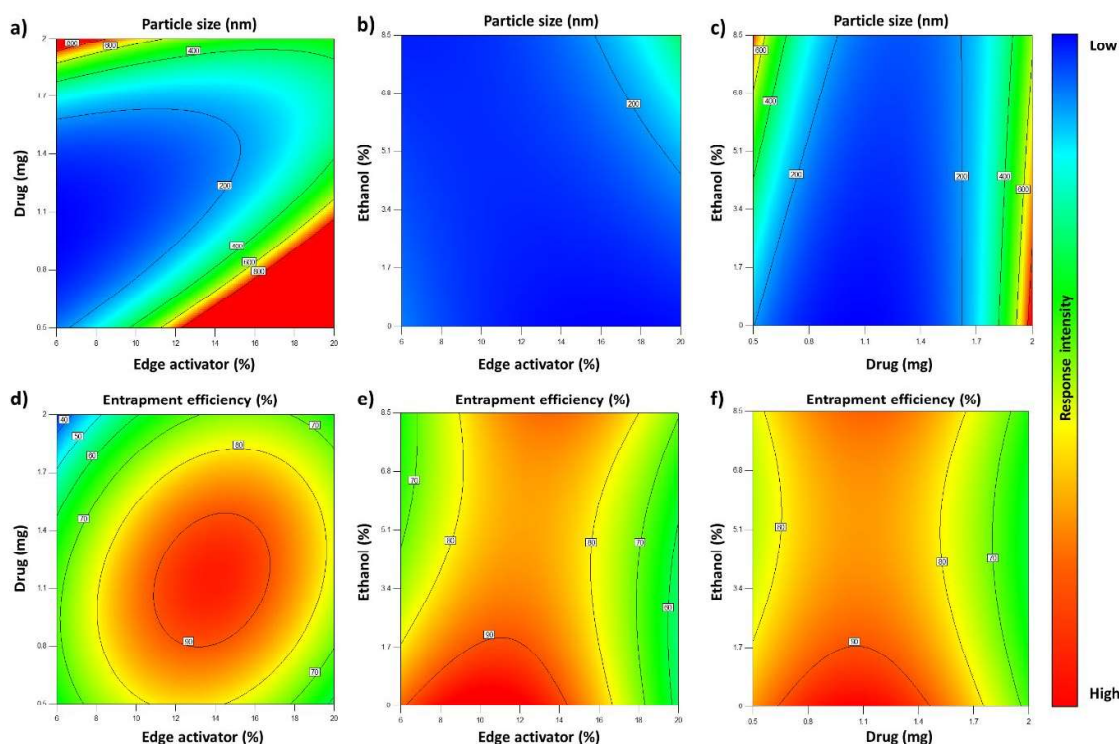


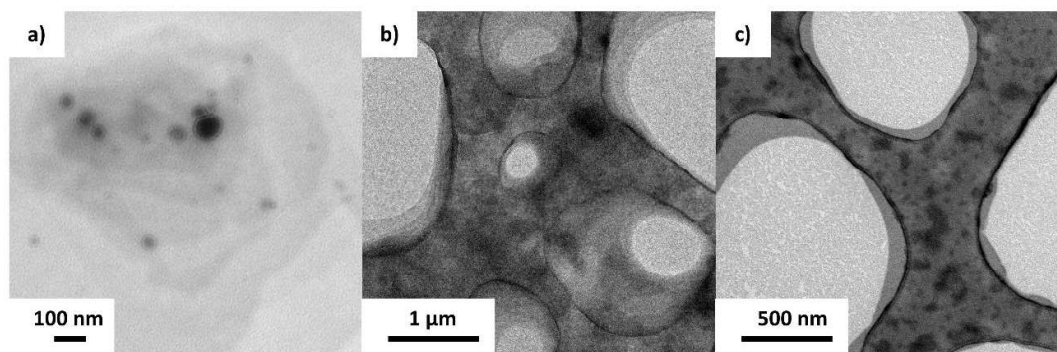
Figure 1. 2D Contour plots showing the effect of the amount of edge activator, drug and ethanol on particle size (a, b, c) and EE (d, e, f).

The predicted and experimental values were in good agreement for particle size and EE. The optimised formulation consisted of 14.13:86.87 (w:w) sodium deoxycholate : soya phosphatidylcholine. The final drug loading after removing the unencapsulated fraction was 0.086 %. The reconstitution buffer was consisted of 91.5 % PBS buffer (pH 7.4) and 8.5 % of ethanol. Even though, a greater EE was obtained with amounts of ethanol below 2% or above 7%, a greater amount of ethanol was chosen to enhance skin permeation. The optimised AmB-TFs resulted in a median particle size of 149 ± 22 nm (D10 of 130 ± 12 nm and a D90 of 168 ± 6 nm), with a zeta-potential of -35.02 ± 2.71 mV and an EE of 93.3 ± 1.9 %. The prediction error was well-below 10 %. No statistical difference was observed between fresh and lyophilised AmB-TFs in terms of particle size and zeta-potential ($p > 0.05$, Student t-test).

Characterisation of optimised AmB-TFs

TEM images of freshly prepared AmB-TFs (Fig. 2a) showed quasispherical particles characterised by a dark core and a lighter layer indicative of the phospholipid bilayer. Reconstitution of freeze dried AmB-TFs resulted in quasi-spherical particles with darker cores (Fig. 2b). However, the phospholipid

1
2
3 bilayer was not as clearly observed as in the freshly prepared AmB-TFs. Similar morphology was
4
5 observed after 28 days of storage at 4 °C (Fig. 2c).
6
7



21
22
23 **Figure 2. TEM micrographs of AmB-TFs;** a) Freshly prepared AmB-TFs stained with 1 % uranyl
24 acetate (Bar: 100 nm); b) Reconstituted freshly prepared freeze-dried AmB-TFs in deionised water
25 stained with 2 % phosphotungstic acid (Bar: 1 µm); c) AmB-TFs after 28 days of storage at 4 °C
26 stained with 2 % phosphotungstic acid (Bar: 500 nm).
27
28

29 **Physicochemical stability of AmB-TFs**

30
31
32 Stability studies showed that AmB-TFs were physicochemically stable for at least one month in liquid
33 state at 4 °C and for at least six months after freeze-drying at 4 °C and 25 °C under desiccated conditions
34 (10 % RH), with a drug content higher than 90 % (Fig. 3a & 3c). The chemical degradation of AmB-
35 TFs was significantly affected when stored at 60 % RH. Particle size of AmB-TFs was maintained over
36 one month without significant differences between 4 and 25 °C storage temperature (Fig. 3b); however,
37 reconstituted freeze dried AmB-TFs showed a tendency for aggregation at all the three tested conditions
38 (4°C, 25°C/10% RH and 25°C/60% RH) (Fig. 3d), being more pronounced at 25 °C and 60 % RH (with
39 2-fold increase in size after 6 months, $p < 0.05$). This indicates that desiccated conditions are necessary
40 to prevent physical instability of freeze dried AmB-TFs.
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

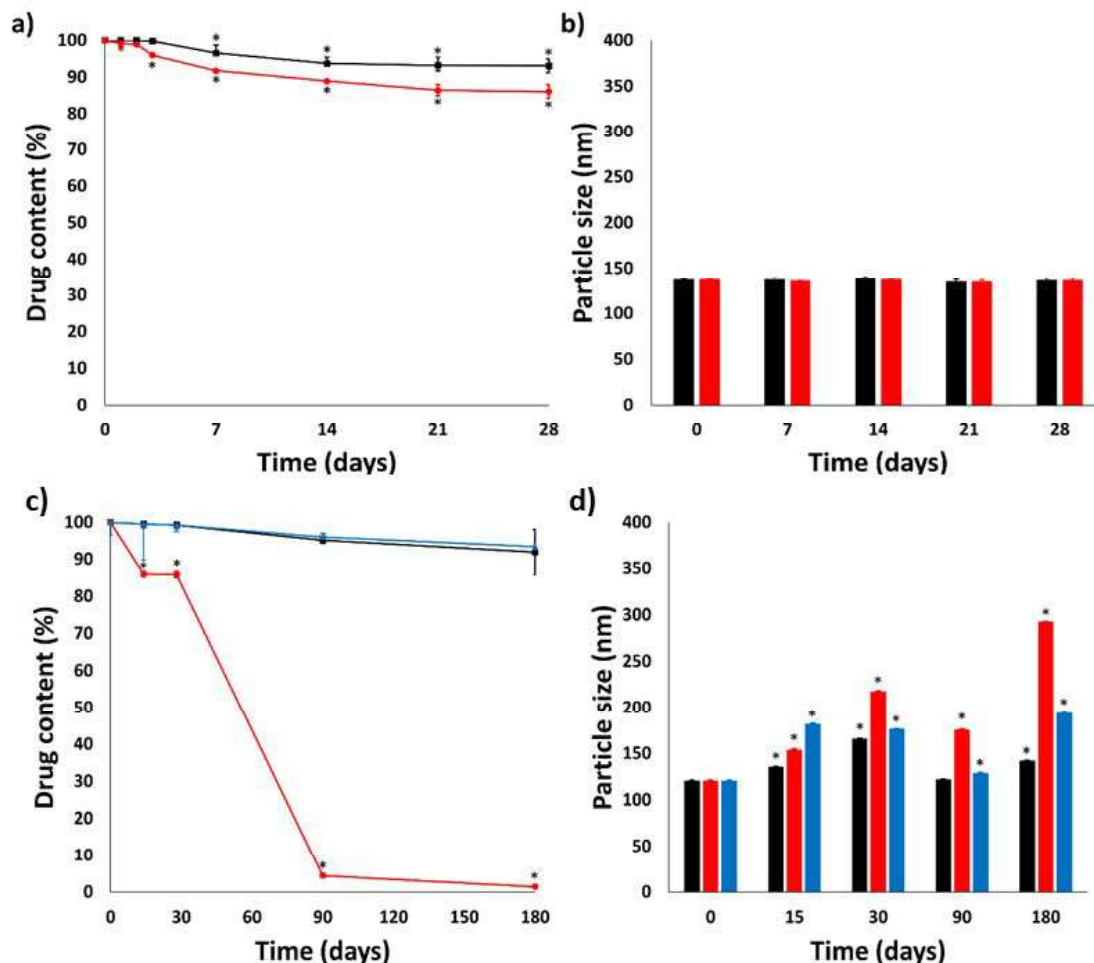


Figure 3. Physicochemical stability of liquid and freeze-dried AmB-TFs: a) Chemical stability of liquid AmB-TFs; b) Physical stability of liquid AmB-TFs. Key: 25 °C (red circles), 4 °C (black squares); *p<0.05 is indicative of statistically significant difference between each time point and time 0 (one-way ANOVA post-hoc Dunnett's test). c) Chemical stability of freeze-dried AmB-TFs; d) Physical stability of freeze-dried AmB-TFs. Key: 25 °C, 10 % RH (black squares), 25 °C, 60 % RH (red circles), 4 °C, 10 % RH (blue triangles); *p<0.05 is indicative of statistically significant difference between each time point and time 0 (one-way ANOVA post-hoc Dunnett's test).

***In vitro* permeability studies**

AmB permeation across Strat-M® membranes was linear for both AmB-TFs and AmB-DMSO. Lag time observed was 9.99 ± 4.59 and 4.86 ± 2.87 minutes for AmB-TFs and AmB-DMSO, respectively. The steady flux over 6 hours for AmB-TFs was 41.18 ± 1.39 $\mu\text{g}/\text{cm}^2/\text{h}$ and 211.06 ± 15.33 $\mu\text{g}/\text{cm}^2/\text{h}$ for AmB-DMSO. It was found that AmB-DMSO had 5.13 times higher permeation than AmB-TFs ($p=0.0018$) across synthetic membranes (Fig. 4a). On the contrary, the two formulations started to permeate immediately across mouse skin, with no lag time. Flux was linear between times 0 to 250

minutes and was $4.91 \pm 0.41 \mu\text{g}/\text{cm}^2/\text{h}$ for AmB-TFs and $5.49 \pm 1.18 \mu\text{g}/\text{cm}^2/\text{h}$ for AmB-DMSO. There were no statistically significant differences at permeation any point ($p > 0.05$) (Fig. 4b). Diffusion for AmB-DMSO was 17-fold lower across mouse skin than in Strat-M[®] membranes, while for AmB-TFs it was only 1.4-fold lower (Table 2). The amount of AmB entrapped in mouse skin after permeation studies was 3.28 ± 0.84 and $25.57 \pm 4.42 \mu\text{g AmB}/\text{cm}^2$ skin for AmB-TFs and AmB-DMSO respectively. This illustrates the potential of TFs to deliver large molecular weight drugs such as AmB across the skin.

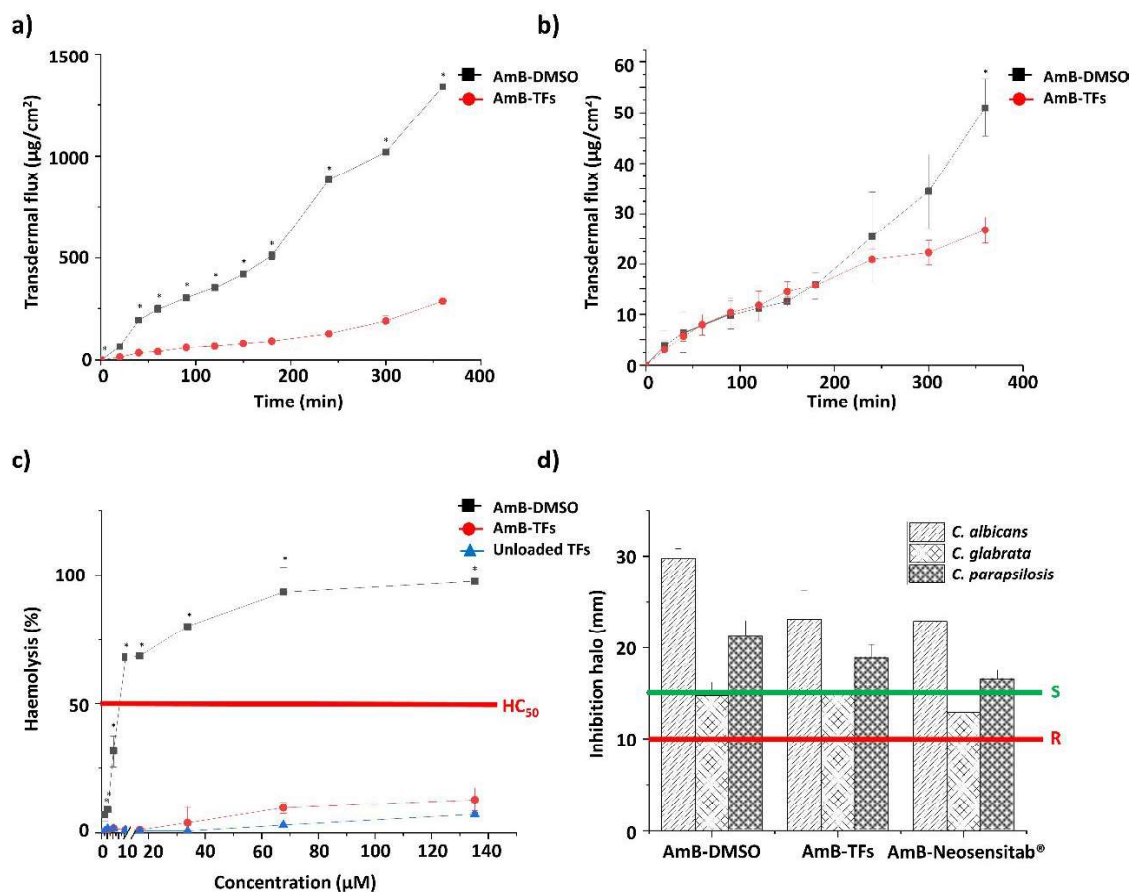


Figure 4. Permeability, toxicity and *in vitro* activity of AmB-TFs: a) Permeability of AmB-TFs and AmB-DMSO across Strat-M[®] membranes; b) Permeability of AmB-TFs and AmB-DMSO across mouse skin; c) Haemolytic toxicity of AmB-TFs, AmB-DMSO and unloaded TFs; d) Antifungal activity of AmB-TFs, AmB-DMSO and AmB-Neosensitabs[®]. Key: AmB-DMSO (black squares), AmB-TFs (red circles), unloaded TFs (blue triangles), concentration that produces 50 % of haemolysis (HC_{50}), sensitivity (S), resistance (R). Statistically significant difference is represented by * ($p < 0.05$) when comparing to AmB-DMSO with other formulations.

Table 2. Permeability and diffusion across Strat-M[®] membranes and mouse skin for AmB-TFs and AmB-DMSO.

| Formulation | Membrane | Permeability (cm/h) | Diffusion x 10 ⁻³ (cm ² /h) |
|-------------|-------------------------------|-------------------------|---------------------------------------------------|
| AmB-TFs | Strat-M [®] membrane | 0.075 | 2.25 |
| | Mouse skin | 8.99 x 10 ⁻³ | 1.6 |
| AmB-DMSO | Strat-M [®] membrane | 0.408 | 12.0 |
| | Mouse skin | 0.011 | 0.711 |

Haemolysis assay

Haemolytic studies for AmB in DMSO showed an HC₅₀ of 10.93 μM, while values 10-fold higher (> 135 μM) were observed for both AmB-TFs and unloaded TFs. This suggests that entrapment of AmB in TFs is able to reduce the haematotoxicity of AmB. (Fig. 4c).

In vitro antifungal activity

AmB-TFs were effective against the three strains of *Candida* spp. assayed (Fig. 4d). Similar to AmB dissolved in DMSO, an inhibition halo greater than 15 mm was obtained for all the three species, indicating that all of them were susceptible to AmB-TFs. Halos <10 mm indicate poor activity while an inhibition halos between 10 and 15 mm demonstrate that the efficacy of the formulation is dose-dependent¹². The lack of diffusion across the agar can result in poorer activity. AmB-TFs showed a good diffusivity capacity across the agar along with a good *in vitro* antifungal activity similar to AmB dissolved in DMSO.

In vitro antiparasitic activity and cytotoxicity against macrophages

L. (L.) amazonensis (MHOM/Br/79/Maria) and *L. (V.) braziliensis* (MHOM/Br/75/M2903) were selected to test the *in vitro* activity of the AmB-TFs formulation as these two species are responsible for most of the cutaneous leishmaniasis (CL) and mucocutaneous leishmaniasis (MCL) in Latin America¹³. The IC₅₀ against the free form of the parasite (promastigotes) was 2.00 ± 0.24 and 3.42 ± 0.15 μM for *L. (L.) amazonensis* and *L. (V.) braziliensis* respectively, while higher IC₅₀ (5.37 ± 0.19 and 7.08 ± 0.34 μM) was observed for the intracellular forms (amastigotes) (Table S3 in SI). The CC₅₀ against J774 macrophages was 33.98 ± 4.02 μM resulting in a SI of 6.3 and 4.8 for *L. (L.) amazonensis* and *L. (V.) braziliensis*, respectively. Compared to the AmB sodium deoxycholate micelles (Fungizone[®]), the AmB-TFs were 3-fold less toxic¹².

Histological studies

Skin treated with AmB-TFs (Fig. 5a-b) or AmB-DMSO (Fig. 5c-d) showed major morphological changes, being more pronounced in the latter. In both cases, disorganization of connective tissue has been observed, which compromised the junction between the epidermis and the dermis, while as well as for the untreated skin, inflammatory cells were not observed.

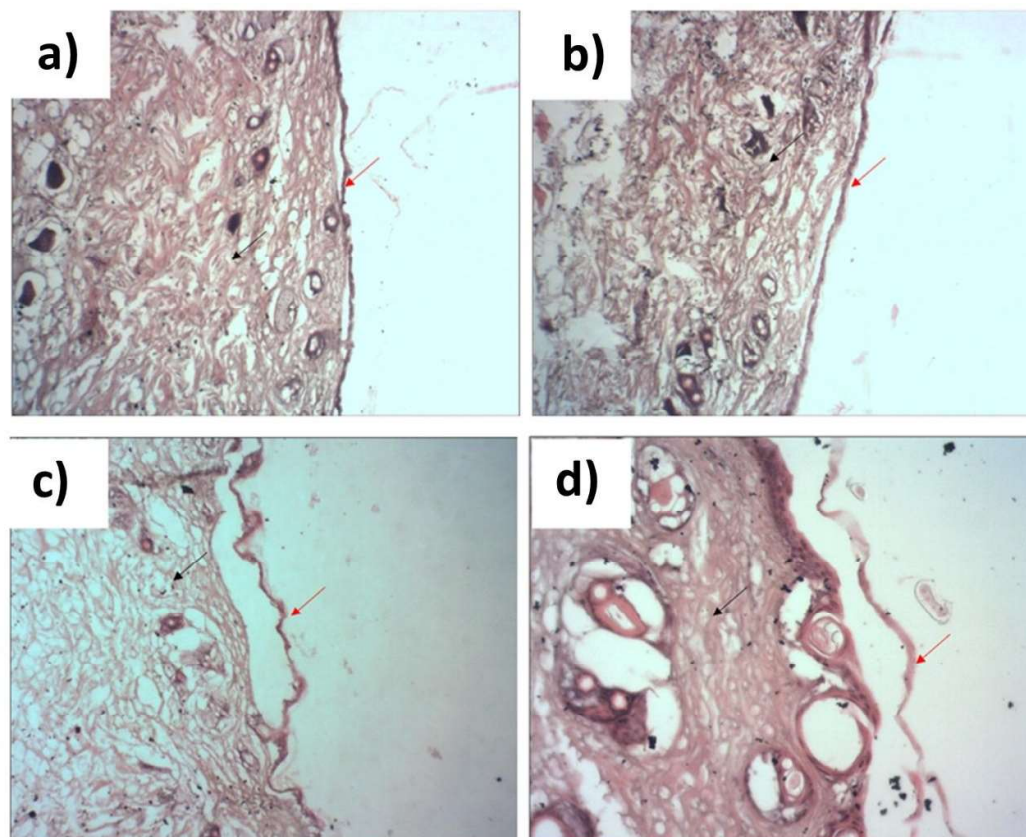


Figure 5. Micrographs of histological studies for treated skin with AmB-TFs and AmB dissolved in DMSO: a) mouse skin after exposure to AmB-TFs, 4x magnification; b) mouse skin after exposure to AmB-TFs, 10x magnification; c) mouse skin after exposure to AmB-DMSO, 4x magnification; d) mouse skin after exposure to AmB-DMSO; 10x magnification.

***In vivo* topical pharmacokinetic studies**

In vivo tape stripping was undertaken to access AmB levels within the SC and dermis after 0.5, 1, 2, 4 and 6 hours of exposure to AmB-TFs or the application of microneedles followed by topical administration of AmB-TFs immediately after which the animals were euthanised. As the thickness of the SC from the back of mice is approximately $15\ \mu\text{m}$ ¹⁴⁻¹⁶, the concentration in the SC ($15\ \mu\text{m} \sim 15$ tapes), dermis ($\sim 12\ \mu\text{m}$) (Fig. 6) and remaining homogenised skin is summarised in Figure 7a. Selected time points for tape stripping were collected after steady state as established ($>1.7\ t_{lag}$)¹⁷. AmB encapsulated within TFs was able to permeate to deeper regions of the skin (Fig. 6a-b). Application of microneedles prior to the topical administration of AmB-TFs resulted in an increase in drug permeation during the first hour, especially in deeper regions of the skin. Application of solid microneedles resulted in transient micropores that facilitate drug delivery across the skin¹⁸, as confirmed by 0.5 and 1 h levels (Fig. 6c-d). However, micropores are known to reseal within 2 h when the skin is not occluded^{19,20} and the overall advantage is lost at later time points. This could also indicate the scar tissue formation limits

AmB permeation as effective surface are for permeation has been reduced. At shorter times (0.5 h), AmB cumulative levels increase linearly, while over time, the permeation process was saturated. Diffusion is easier within the first 4-5 strips, while the diffusion is hindered in deeper skin areas as water osmotic gradient is less steep. Longer periods of AmB-TFs exposition to the skin resulted in greater amounts of drug accumulated in the skin (Fig. 7a). Bearing in mind the *in vitro* activity against amastigotes, effective concentrations are obtained after one hour from topical administration, and possibly even earlier (0.5 h) if microneedles are applied previous to topical application. However, the use of metallic microneedles did not result in statistical significant increase in AmB in the deeper skin layers at any time point, which means that transdermal delivery of AmB is unlikely (Figure 7a).

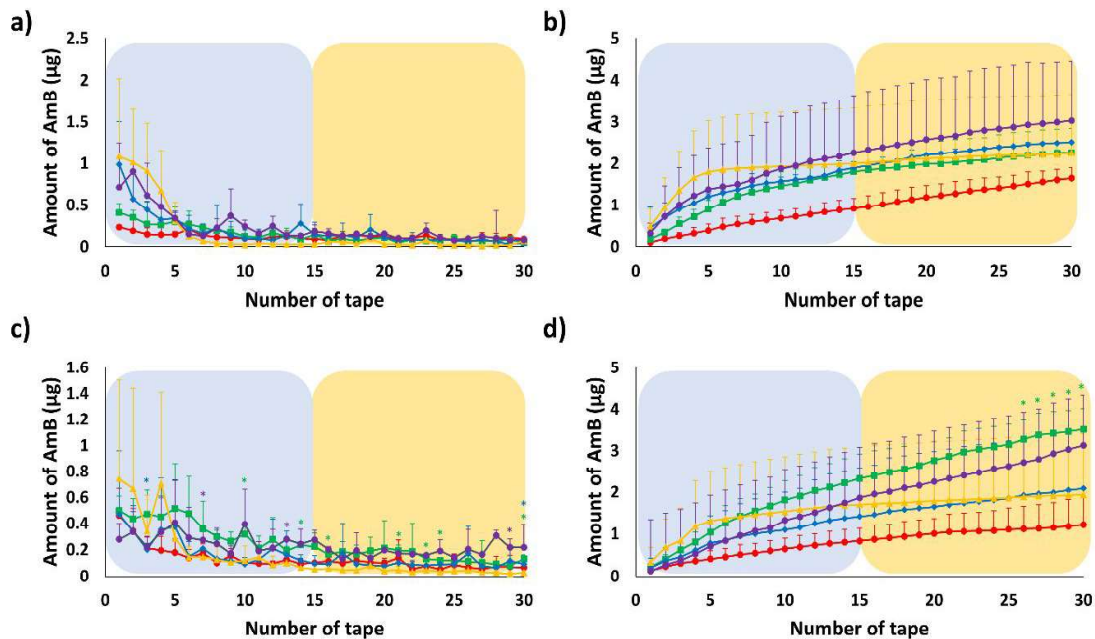
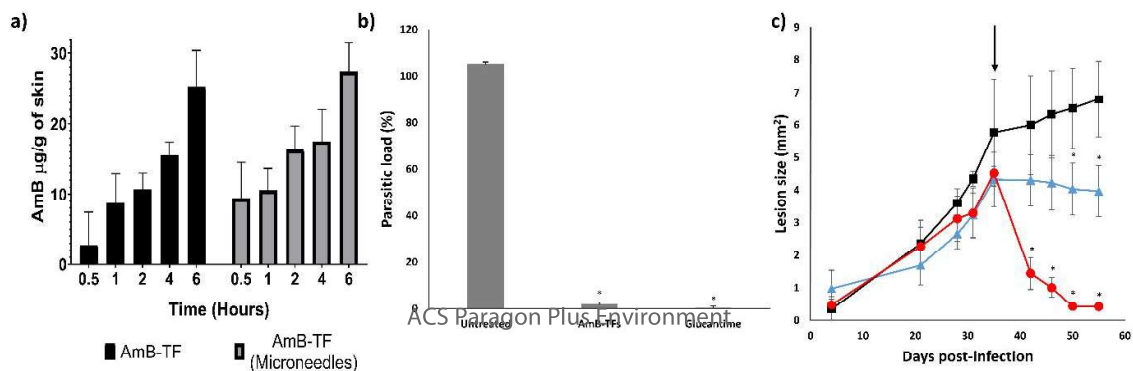


Figure 6. Averaged amount of AmB per tape strip (a, c) and cumulative amount of AmB (b, d) in mouse skin after 0.5, 1, 2, 4 and 6 h of post-administration without the application of microneedles (a, b) and after the utilization of microneedles (c, d). Key: 0.5 h (red circles), 1 h (green squares), 2 h (blue diamonds), 4 h (yellow triangles), 6 h (purple circles). The blue and orange panels represent the stratum corneum and the evaluated skin once the stratum corneum is removed, respectively. Statistically significant differences are represented by * ($p < 0.05$, one way-ANOVA post-hoc Tukey's test).



1
2
3 **Figure 7. a) Amount of remaining AmB in the skin after removal of 30 tape-strips after the topical**
4 **AmB-TFs administration (black bars) and topical AmB-TFs administration after application of**
5 **microneedles (grey bars); b) *In vivo* antiparasitic activity (parasitic load) of AmB-TFs (0.5 mg/ml,**
6 **20 mg of formulation/day, once daily topically applied) and Glucantime® (50 mg/kg, once daily 25**
7 **µl intralesionally administered) in experimental cutaneous leishmaniasis caused by *L. (L.)***
8 ***amazonensis*; c) Evaluation of lesion size during the course of the infection.** Key: untreated animals
9 (black squares), AmB-TFs (blue triangles), Glucantime® (red circles). Arrow indicates the onset of
10 treatment. Statistically significant differences between treated and untreated animals is represented by
11 * ($p < 0.05$, Mann-Whitney U test).

12 ***In vivo* antiparasitic activity**

13
14
15
16
17
18
19
20 *In vivo* antiparasitic activity of topically administered AmB-TFs is illustrated in Figure 7b-c. The
21 administration of topical AmB-TFs for 10 days resulted in a decrease in parasitic load of 98.24 ± 1.54
22 % similar to the decrease achieved with intralesionally administered Glucantime® (99.78 ± 0.31 %)
23 with a p-value > 0.05 (Fig. 7b, Table S4 in SI). When evaluating the lesion size, a decrease was observed
24 for the Glucantime® and AmB- TFs from the sixth measurement (one month and a half post-infection
25 and seven days after the beginning of the treatment). The untreated group showed a linear progression
26 of the lesion size over time. The healing of the lesion was faster in animals intralesionally treated with
27 Glucantime®, while in the case of AmB-TFs, the reduction in the lesion size was only significant at the
28 eighth measurement (six days after the end of the treatment) (Fig. 7c). These results suggest that longer
29 administration periods or potentially twice daily administration of topical AmB-TFs could lead to a
30 total remission of the cutaneous lesion. From a practical point of view, AmB-TFs could be advantageous
31 compared to Glucantime® as the latter is painful and requires intralesional administration in clinical
32 settings limiting patient compliance, especially in developing countries ²¹.

33 **DISCUSSION**

34
35
36
37
38
39
40
41
42
43
44
45
46
47
48 Here, we describe a topical AmB transfersomal formulation able to effectively deliver AmB across the
49 stratum corneum and reach drug therapeutic levels in the epidermis to elicit a pharmacological effect as
50 evidenced by *in vivo* pharmacokinetic and efficacy studies for the treatment of fungal and parasitic
51 infections. For the latter, there is a strong need for topical therapies for CL and MCL, particularly for
52 the milder and most common cases with up to 4 ulcers not exceeding 3 cm in diameter ¹. However, drug
53 formulations for topical application have not met the expected impact. Paromomycin-based ointment
54 marketed in the Middle East was not effective against New World parasite species ^{22, 23}, while a cream
55 containing 3 % of AmB (Anfoleish) showed poor efficacy in a clinical study in Colombian CL patients
56
57
58
59
60

1
2
3
4
5
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

⁵ resulting in a range of adverse effects such as itching, redness, peeling dryness and irritation of the skin ⁶. Thus, there is still an unmet clinical need for AmB topical formulations able to localise high amounts of AmB in the skin for fighting these infections.

DOE studies informed the design of the TFs in terms of drug loading, small particle size and colloidal stability prepared from generally regarded as safe excipients (GRAS). The choice of the edge activator is critical in the design of TFs and sodium deoxycholate was chosen as it is known to be a good solubiliser for AmB as well as a proven edge activator to ensure critical fluidity required for permeation of TFs ⁸. Optimising the ratio between sodium deoxycholate and AmB was critical as there is an inverse relationship between the amount of sodium deoxycholate and particle size (Fig. 1). It is worth to highlight that sodium deoxycholate is the excipient traditionally utilised to solubilise AmB in Fungizone[®], in which dimeric AmB is formulated in a molar ratio 1:2 drug:excipient ²⁴. Although there are reports of skin irritation for NaDC when skin is exposed to this water soluble ionic surfactant, sodium deoxycholate stabilized transfersomes have not shown any signs of dermatological toxicity after topical application as supported by *in vitro* studies and clinical studies ^{8, 25}.

Prepared AmB-TFs were able to solubilise high amounts of AmB comparable to those previously reported ¹¹. Sodium deoxycholate was also preferred over non-ionic surfactants, such as Tween[®] 80 or Span[®] 80 ^{8, 11, 26, 27} due to the greater EE obtained in preliminary studies. AmB-TFs exhibited an EE close to 95 % which can be attributed to the combination of soya phosphatidylcholine and sodium deoxycholate (86.87:14.13 w:w) which facilitates apolar interactions within the hydrophobic regions of both molecules as well as electrostatic interactions between the carboxylic group of the sodium deoxycholate and the primary amine of the AmB. The optimised formulation exhibited an AmB concentration of 0.086 % w/v. Higher drug concentrations could be achieved but resulted in drug precipitation and lower EE as well as vesicle aggregation. For this reason, existing drug loading was preferred to the expense of greater EE in order to ensure a small particle size (~150 nm). TEM images confirmed quasi-spherical morphology of similar particle size with a clear bilayer surrounding an aqueous core.

One of the advantages of the optimised AmB-TFs is their enhanced physicochemical stability making their use feasible in developing countries without the need of cold transport chain. As TFs are typical aqueous suspensions, to prolong their stability, we also developed a lyophilised formulation. Freeze-dried AmB-TFs showed a good physicochemical stability (> 90 % drug content and particle size < 200 nm) over six months at 4 and 25 °C under desiccated conditions. Upon reconstitution, liquid AmB-TFs were stable over 30 days at 4 °C and at least over one week at 25 °C. This stability is superior than those reported in the marketed formulations, AmBisome[®] and Fungizone[®] (one day at 25 °C and one week under refrigerated conditions) ²⁸.

1
2
3
4
5
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

In vitro permeation studies across Strat-M[®] membranes (synthetic ultrafiltration membranes composed of two layers of polyether sulfone on top of one layer of polyolefin)²⁹⁻³¹ showed AmB-TFs had a lag time of 9.99 ± 4.59 minutes, while AmB-DMSO 4.86 ± 2.87 minutes. The steady state flux was 5.03-fold lower for AmB-TFs. These membranes are constructed of two layers of polyether sulfone, resistant to diffusion, on top of one layer of polyolefin that is, open and diffusive. These polymers are able to create a porous structure with a gradient across the membrane in terms of pore size and diffusivity. The porous structure is impregnated with a proprietary blend of synthetic lipids, imparting additional skin-like properties. These membranes mimicking skin were previously shown for low molecular compounds with high lot-to-lot reproducibility^{30, 31} and recently showed to have close similarity to human skin for high molecular weight drugs such as AmB²⁹. However, across mouse skin, no statistical significant differences were found in the permeation rate across mouse skin between AmB-TFs and AmB-DMSO, presenting a similar steady-state flux during the first 4 hours as a result of the good permeability of the TFs across the skin. Flux was 6-fold and 4-fold higher than other AmB liposomal and transfersomal formulations, respectively, described previously across rat skin¹¹. The latter transfersomal formulation contained soya phosphatidylcholine, cholesterol and NaDC in a molar ratio of 7:3:1. Flux was also similar to the flux across rat skin of AmB ethosomal preparations that contained a higher percentage of ethanol to the one included in our TFs²⁹. However, AmB ethosomes exhibited a lag time across rat skin of 1.5 hours, while AmB-TFs did not show any lag time in biological skin, indicating that higher amount of ethanol would delay drug release²⁹. This would be advantageous considering that an immediate release would provide a quicker permeation and, thus, a faster effect of the drug.

AmB-TFs illustrated *in vitro* efficacy in New World leishmaniasis species with comparable IC₅₀ to previously studied³² and *Candida* spp.³³. Higher concentrations of AmB were required to inhibit growth of amastigotes in comparison with promastigotes, bearing in mind that the first form of the parasite is located inside macrophages and hence, AmB molecules have to permeate the macrophage membrane in order to reach the parasite reservoir. However, it is key that the drug is selectively more active for parasites than for macrophages. AmB-TFs IC₅₀ in amastigotes were higher than in previous reports³⁴. Differences in origin of murine macrophages which could potentially result in differences in number of available LDL receptors could explain differences in uptake and thus activity, while effects of protein binding, aggregation state between them can potentially explain observed differences^{35, 36}. Additionally, lack of a clear water osmotic gradient *in vitro* could limit permeability in macrophages^{2, 35-38}. However, low *in vitro* IC₅₀ values do not overcome challenges posed by the SC *in vivo* and *in vitro* previously tested results are not indicative of clinical scenario. TFs demonstrated a selectivity index towards amastigotes compared to mammalian macrophages that allows their clinical translation³⁹. This is a therapeutic advantage considering that a limited toxicity allows a higher drug administration dose and hence, higher chance to eradicate the parasites in a multiple dose regime. Entrapping AmB in TFs

1
2
3 reduced the haemolytic effects of AmB, while after 6 hours of skin exposure little if any inflammation
4 was histologically observed. No signs of toxicity was also visible after *in vivo* application of AmB-TFs
5 in infected mice.
6
7

8
9 In our study, *in vivo* topical bioavailability of the formulation in mice was also evaluated. To the best
10 of our knowledge, this is the first time that the pharmacokinetic profile of AmB loaded in TFs is studied.
11 AmB encapsulated in TFs was able to cross the stratum corneum and reach deeper regions of the skin
12 at concentrations above the IC₅₀ for *L. (L.) amazonensis* and *L. (V.) braziliensis*, but also below the CC₅₀
13 for macrophages. From a clinical point of view, this is especially advantageous bearing in mind that
14 parasites are located in the epidermis and dermis ⁴⁰. The use of microneedles prior the administration
15 of AmB-TFs resulted in enhanced drug permeability in SC and dermis up to two hours post-
16 administration. This was in good agreement with studies by other authors under non-occlusive
17 conditions which show that the formed pores heal within two hours, while healing is delayed for up to
18 several days depending on the geometry of the applied microneedles under occlusion ^{14, 41, 42}.
19
20
21
22
23
24

25 The efficacy of AmB-TFs was also demonstrated *in vivo*, where the parasitic load was reduced greater
26 than 98 % after once a day administration for 10 days, exhibiting the same efficacy (p-value <0.05) as
27 intralesionally administered antimonials. The use of microneedles prior to the AmB-TFs topical
28 administration enhanced even further the AmB permeation during the first hour post-application.
29 Previous studies have demonstrated that drug permeability is enhanced in *Leishmania*-infected skin ¹¹.
30 The high efficacy demonstrated by AmB-TFs could also be explained by the fact that trans-epidermal
31 water loss (TEWL) is usually around 2.5-fold higher on skin infected with *Leishmania* spp. ⁴³ and is
32 associated to damaged epidermal and dermal skin layers and reduced density of collagen and
33 effectiveness of the barrier function of skin ⁴⁴. As TFs permeation is driven by the water osmotic
34 gradient and *Leishmania* infected skin is dryer, it is likely that the gradient for TFs permeation is steeper
35 in infected animals and potentially patients. This can potentially explain the enhanced efficacy of our
36 AmB-TFs formulation across infected skin.
37
38
39
40
41
42
43
44

45 Two alternative AmB-TFs semisolid formulations were also prepared by mixing at 1:1 w:w the AmB-
46 TFs with different gelling agents, Carbopol® 940 (at 8 %) and Metolose® 1500 (combination of
47 methylcellulose and hypromellose at 4 %) ⁴⁵. However, the *in vitro* permeation across the skin was
48 limited compared to the liquid formulation probably related to a hindered released from the gel (data
49 not shown). AmB ethosomal gel (1 % w/w) prepared with Carbopol® 934 (1.5 % w/w) have been shown
50 to maintain a high flux in previous reports ²⁹. Further studies are needed to establish the concentration
51 of the gelling agent needed for optimal permeability. The intralesional administration of the AmB-TFs
52 is also feasible if required in severe cases of CL. A liquid formulation would be also beneficial from
53 patients suffering from fungal skin infections disseminated along larger regions of the body.
54
55
56
57
58
59
60

CONCLUSIONS

Our AmB-TFs showed enhanced *in vitro* permeation across Strat-M[®] and mouse skin and elicited therapeutic levels after *in vivo* administration as confirmed by tape stripping and reduction in parasite number in infected mice. Our formulations prepared from GRAS excipients showed improved safety according to haemolysis, cytotoxicity and histological studies and are thermally stable without the need for a cold transport chain. This formulation is readily translatable as a good therapeutic alternative to current treatments for CL and fungal infections in developed and developing countries.

METHODS

Materials

AmB ($\geq 98\%$) was procured from North China Pharmaceutical Huasheng Co (Hebei, China). Phosphatidylcholine (Lipoid S100[®]) was donated from Lipoid GmbH (Ludwigshafen, Germany). Sodium deoxycholate, other chemicals and solvents, as well as Roswell Park Memorial Institute 1640 medium (RPMI-1640) utilized in the culturing of *Leishmania* parasites, were obtained from Sigma-Aldrich Chemie GmbH (Madrid, Spain) and were at least ACS grade. The rest of the materials were purchased as follows: ethanol 96° (Alcoholes Aroca S.L., Madrid, Spain), Strat-M[®] membranes (Merck KGaA, Darmstadt, Germany), Triton X[®]-100 (Sigma-Aldrich Co, St. Louis, USA), Sabouraud dextrose agar (Becton, Dickinson and Co., New Jersey, USA), Müller-Hinton agar (Laboratorios Conda S.A., Madrid, Spain), glucose (Panreac Química S.A.U., Barcelona, Spain) and sterile 0.9 % sodium chloride (Laboratorios ERN, S.A., Barcelona, Spain)

Design of experiment (DOE) of AmB-TFs

A three-level Box-Behnken model was selected to obtain an optimised TFs formulation. DesignExpert[®] 10 software (Stat-Ease Inc., Minneapolis, USA) was utilised to establish the high and low levels of the design. The concentration of edge activator (sodium deoxycholate), the amount of AmB and the percentage of ethanol used to reconstitute the dry film were the chosen factors (independent variables), while encapsulation efficiency (EE), particle size and zeta potential were the selected responses (dependent variables) for optimisation. Ranges of each factor are described in Table 3. Seventeen formulations were prepared using different combinations of the factors. The batch size was kept constant (200 mg in 2 mL). The amount of AmB and edge activator was added based on the DOE (Table 2) and the amount of lipid was calculated as the remaining till 200 mg total amount.

Table 3. Selected factors and levels to implement the Box-Behnken design of experiments for the optimisation of the AmB-TFs formulation.

| Factor | Levels | | |
|-------------------------------------|--------|--------|------|
| | Low | Medium | High |
| Concentration of edge activator (%) | 6 | 13 | 20 |
| Amount of drug (mg) per 2 ml batch | 0.5 | 1.25 | 2 |

| | | | |
|--------------------------------------------------------|---|---|-----|
| Percentage of ethanol in the reconstitution buffer (%) | 0 | 4 | 8.5 |
|--------------------------------------------------------|---|---|-----|

Other variables involved in the manufacturing process were kept constant through the 17 runs such as: rotaevaporation time (30 min), reconstitution volume (2 mL) and probe sonication time.

Optimisation of AmB-TFs formulation and validation of the model

Mathematical modelling was carried out by multiple linear regression analysis (MLRA). Only the statistically significant coefficients ($p < 0.05$) were considered in framing the polynomial equations, and the model was evaluated by analysing the p-value and the determination coefficient (R^2). Response surface analysis was carried out employing 2D and 3D plots for understanding the relationship among the amount of edge activator, drug and ethanol on particle size and EE. The prognosis of the optimum formulation was conducted by numerical optimization and desirability function with the aim of maximising EE and particle size ranging from 100 to 300 nm. Validation of the QbD methodology was performed by comparing the predicted responses with the experimental ones.

Preparation of AmB-TFs

AmB-TFs were prepared by the thin film hydration method. AmB (1.82 mg), phosphatidylcholine Lipoid S100[®] (171.74 mg) and NaDC (28.26 mg) were dissolved in methanol (20 mL) in a round-bottom flask. Solvent was evaporated protected from light under vacuum using a rotaevaporator RV 06-ML (Janke & Kunkel Ika-Labortechnik, Staufen, Germany) and a vacuum pump Vac[®] V-500 (Büchi Labortechnik, Flawil, Switzerland) controlled by a vacuum controller B-721 (Büchi Labortechnik, Flawil, Switzerland) till a dry film was obtained at 43 °C and 250 r.p.m.. The film was hydrated by adding 2 mL of a mixture of phosphate buffered saline (PBS) pH 7.4 (295.8 mOsm/L) and ethanol (91.5:8.5 v:v) under rotation using the rotaevaporator over 30 minutes while being protected from light. The resulting suspension was then bath sonicated (150 Watts, P Selecta Ultrasons-H, Barcelona, Spain) for 30 minutes and probe sonicated (10 Watts, two cycles of 10 seconds with 50 seconds in between to avoid overheating, Branson Sonifier 250, Emerson Industrial, Connecticut, USA). The formulation was centrifuged at room temperature (6,000 rpm, 15 min) using a Universal 32[®] centrifuge (Hettich Zentrifugen, Tuttlingen, Germany) to separate the unencapsulated AmB.

Lyophilisation of optimised AmB-TFs formulation

Mannitol was added to the liquid optimised AmB-TFs formulation as a cryoprotectant. Mixtures were frozen at -40 °C overnight and freeze-dried at -50 °C and a pressure of 0.2 bar for 24 hours in a LyoQuest freeze-drier (Azbil Telstar, S.L., Terrassa, Spain). The final solid concentration in the lyophilised formulation was 11.6 % w/v, containing 0.923 mg of AmB, 173.1 mg of phosphatidylcholine, 26 mg of sodium deoxycholate and 33.35 mg of mannitol.

Characterisation of the optimised AmB-TFs

Particle size and zeta potential were measured in freshly prepared AmB-TFs using a Zetatrac Ultra (Microtrac Inc, Pennsylvania, USA) analyser. Particle size was measured by dynamic light scattering (DLS). Prior to measurements, samples were diluted with deionised water (1/100 v/v).

Morphology of the optimised formulation was evaluated using transmission electron microscopy (TEM) (S2.1 in SI). EE was measured after centrifugation at 6,000 rpm for 15 min in a Universal 32[®] centrifuge (Hettich Zentrifugen, Tuttlingen, Germany) at room temperature. The supernatant was diluted with methanol (1/100, v/v). The absorbance was measured using a PharmaSpec[®] UV-visible spectrophotometer (Shimadzu, Kyoto, Japan) between 300 and 450 nm wavelength to ensure all the drug was in the monomeric state¹. The absorbance at 406 nm was recorded. EE was calculated using the following equation⁴⁶ (Eq. 4):

$$EE (\%) = \frac{A-B}{A} \times 100 \quad (\text{Eq. 4})$$

where A was the absorbance at 406 nm of the formulation after probe sonication before centrifugation and B was the absorbance at 406 nm of the formulation after centrifugation.

Physicochemical stability of AmB-TFs

Freshly prepared AmB-TFs were diluted with PBS pH 7.4 313 mOsm/L (1/15 v/v), consisting on NaCl (8 g/L), KCl (0.2 g/L), Na₂HPO₄ (1.44 g/L) and KH₂PO₄ (0.24 g/L). The batch was then divided in different vials containing 1 mL (79.8 μg of AmB mL⁻¹) each. Half of the vials were lyophilised as described above. Both formulations were stored at 4 or 25 °C. The effect of relative humidity (RH) on the stability of lyophilised formulation was assessed at 25 °C that was controlled at 10 and 60 % using different saturated salt solutions⁴⁷. Lyophilised formulations were placed in uncapped vials. Prior to analysis, freeze dried samples were reconstituted with 1 ml of deionised water. At different time points, samples were withdrawn and particle size and drug content by HPLC⁴⁸ were measured.

In vitro permeability studies

Male BALB/c untreated mice (8 weeks old, 26-28g, Harlan, UK) were euthanised and hair was trimmed prior skin being freshly excised and frozen in -50 °C in flat closed plastic bags. The skin was thawed and shaved, then suspended in 60 °C deionised water for 30 seconds to manually remove the underlying muscle tissue and hypodermis¹⁴. Then the skin was placed flat in plastic bags and stored in -50 °C freezer till further use. When needed, the skin was thawed in receptor fluid buffer prewarmed at 37 °C prior use. Strat-M[®] membranes required no preparation.

Diffusion studies of optimised AmB-TFs (0.086 % w/v) and equivalent AmB in dimethylsulfoxide (DMSO) at 0.086 % w/v were performed using vertical diffusion Franz Cells (Soham Scientific,

Loughborough, UK). The diffusion diameter of each Franz cell was measured using a caliper (± 0.01 mm) and the surface area ranged between 5.29-5.34 cm². Strat-M[®] membranes (Merck KGaA, Darmstadt, Germany) or mouse skin were placed on receptor compartment with the stratum corneum facing upwards and a stirring bar (3 x 5 mm) was added to each Franz Cell's receptor compartment and then filled completely with 4 % w/v sodium deoxycholate in PBS (pH 7.4) to ensure sink conditions. Strat-M[®] membranes (synthetic models for transdermal diffusion testing) required no preparation according to the recommendations of the manufacturer⁴⁹. The donor compartment, the membrane or skin, and the receptor compartment were tightly sealed using ParaFilm[™] and clamped together. PBS (1 mL) was added into the donor compartment and then placed into a water bath at 37 °C (Tempette Junior TE-8J, Techne, Staffordshire, UK) for 30 minutes under magnetic stirring (Fisherbrand, Leicestershire, UK). After 30 minutes, the PBS and receptor media were removed for analysis and the receptor compartment filled with fresh and prewarmed 4 % w/v sodium deoxycholate in PBS (pH 7.4). AmB-TFs or AmB in DMSO (0.6 g of each formulation at an AmB concentration of 0.086 % w/v equivalent to an AmB dose utilized of 0.517mg) were added to the donor chamber. At selected time points (0, 20, 40, 60, 90, 120, 150, 180, 240, 300 and 360 min), 0.5 ml of the receptor medium was taken using a syringe and immediately refilled with 0.5 ml of fresh media. AmB concentration was quantified in the samples using a validated HPLC method⁴⁸ (Jasco Inc., Maryland, USA) with a lower limit of detection (LoD) of 0.19 $\mu\text{g mL}^{-1}$.

The cumulative amounts of AmB permeated through the Strat-M[®] membrane and the mouse skin were plotted as a function of time⁵⁰. Regression analysis was used to calculate from the slopes and intercepts of the linear portion of each graph. The following equation (Eq. 5) was applied to each formulation to calculate the steady-state flux:

$$J_{ss} = \frac{dC}{dX} * \frac{1}{A} \quad (\text{Eq. 5})$$

where J_{ss} is the steady-state flux ($\mu\text{g}/\text{cm}^2/\text{h}$), dC/dX is the amount of AmB permeating the membrane over time ($\mu\text{g}/\text{h}$) and A is the surface area of contact of the formulation⁵¹. The permeability coefficient (P) was calculated by using equation 6:

$$P = \frac{J_{ss}}{cd} \quad (\text{Eq. 6})$$

where cd is the amount of drug applied in donor compartment (0.6 g of formulation equivalent to 0.517 mg of AmB). Diffusion coefficient was calculated by using the following equation:

$$D = P h \quad (\text{Eq. 7})$$

where h is the thickness of the membrane (0.62 ± 0.08 mm)⁵².

1
2
3 After permeability studies with mouse skin, skin was cleaned with a cotton bud to remove excess of
4 formulation. Samples were cut in two halves. One half was fixed using 4 % paraformaldehyde (pH 7).
5 In the other half, AmB was extracted (3 times) using 3 ml of buffer with 4 % sodium deoxycholate:
6 methanol (1:1 v:v). After each extraction, the homogenate was vortexed (2 min) and centrifuged (8,000
7 rpm, 10 min, room temperature) and supernatant was collected and transferred into HPLC vials. The
8 supernatant was analysed by a validated HPLC method⁴⁸. Statistical analysis was performed by 2-tail,
9 unequal variance, student t-test on flux at each time point.
10
11
12
13

14 **Histological studies**

15
16
17 Mouse skin samples exposed to AmB-TFs, AmB-DMSO for 6 hours in the Franz Cells, as well as
18 pretreated skin that had not been exposed to any formulation at all were fixed separately with
19 paraformaldehyde (4 %, pH 7.4) and refrigerated (2-8 °C). Histological studies were performed as
20 previously described (S2.2 in SI)^{14, 50, 53}.
21
22
23

24 **Ex vivo red blood cells haemolysis assay**

25
26 *Ex vivo* haemolytic activity of AmB was determined using blood taken from a healthy human donor
27 (female, 32 years old, haematocrit: 45 %) as previously described with few modifications (S2.3 in SI)
28⁵⁴. RBCs (100 µL, 4 % w/v) were added to a 96-well plate followed by AmB-TFs (100 µL) diluted to
29 various concentrations between 270 to 4 µM. AmB-unloaded TFs in PBS were diluted at the same
30 concentrations and were also tested. PBS (pH 7.4) and Triton X[®]-100 diluted to 20 % in PBS (pH 7.4)
31 were used as negative and positive controls respectively. AmB dissolved in DMSO was also used as a
32 control. Haemolysis at each concentration was calculated by using the following equation (Eq. 8):
33
34
35
36
37

$$38 \text{ Haemolysis (\%)} = \frac{\text{Abs}(s) - \text{Abs}(\text{PBS})}{\text{Abs}(\text{Triton}) - \text{Abs}(\text{PBS})} \times 100 \quad (\text{Eq. 8})$$

39
40
41 where Abs(s) is the average absorbance of the sample at each concentration tested, Abs (PBS) is the
42 average absorbance of the negative control, and Abs (Triton) is the average absorbance of the positive
43 control. Data were analysed using Compusyn[®] (Combosyn Inc, New Jersey, USA) software and HC₅₀
44 (concentration needed to haemolyse 50 % of erythrocytes) was obtained.
45
46
47

48 **In vitro antifungal activity**

49
50 The *in vitro* antifungal activity of AmB was determined according to European Pharmacopeia standards
51 in three different species of *Candida* spp.: *C. albicans*, *C. glabrata* and *C. parapsilosis* (S2.4 in SI)¹².
52 One-way ANOVA was undertaken using Minitab[®] 16 software.
53
54

55 **In vitro antiparasitic activity**

56
57 Two species of *Leishmania* spp., *L. (L.) amazonensis* and *L. (V.) braziliensis* were cultured in
58 Schneider's insect medium (Sigma-Aldrich Co, St. Louis, USA) at 26 °C supplemented with 20 % heat-
59
60

1
2
3 inactivated foetal bovine serum (FBS) (Sigma-Aldrich Co, St. Louis, USA), penicillin (100 IU/mL) and
4 streptomycin (100 µg/mL) in culture flasks (25 mL) ^{55, 56}. Two different assays against promastigotes
5 and amastigotes were carried out with resazurin, following methods previously described in literature
6 (S2.5 in SI) ⁵⁶. The efficacy of each compound was determined by calculating the IC₅₀ (concentration
7 of formulation needed to inhibit 50 % growth) ⁵⁶.
8
9

10 ***In vitro* macrophage cytotoxicity**

11
12 Macrophage cytotoxicity was determined in J774 murine macrophages (S2.6 in SI) ^{55,56}. The results
13 were expressed as CC₅₀ (concentration that produced cytotoxicity in 50 % of macrophages). Selectivity
14 index (SI) was calculated to evaluate the relationship between efficacy and toxicity for AmB-TFs using
15 the following equation (Eq. 9):
16
17
18
19

$$20 \quad SI = \frac{CC_{50}}{IC_{50}} \quad (\text{Eq. 9})$$

21 **Animals for efficacy and topical pharmacokinetics studies**

22
23 Mice were obtained from the Medical School of University of São Paulo, Brazil. The studies were
24 carried out in accordance with the recommendations detailed in the Guide of the Care and Use of
25 Laboratory Animals of the Brazilian National Council of Animal Experimentation
26 (<http://www.cobea.org.br>). The protocol was approved by the Ethics Committee of Animal Experiments
27 of the Institutional Committee of Animal Care and Use at the Medical School of the University of São
28 Paulo (CEUA 056/16). Mice were housed according to the standards of the Committee of Animal
29 Welfare and allowed access to food and water *ad libitum* throughout the study under a 12 h light cycle.
30 The animals were anesthetized with intraperitoneal sodium thiopental (1 mg/200 µL).
31
32
33
34
35
36
37
38

39 **Efficacy studies in *L. (L.) amazonensis* infected mice**

40
41 *L. (L.) amazonensis* (MHOM/BR/73/M2269) was kindly provided by Prof. Dr. Fernando T. Silveira
42 from the cryobank of the “Leishmaniasis Laboratory Prof. Dr. Ralph Laison”, Department of
43 Parasitology, Ministry of Health, Evandro Chagas Institute (Belém, Pará – Brazil). Species were
44 identified using monoclonal antibodies and isozyme electrophoretic profiles at the Leishmaniasis
45 Laboratory of the Evandro Chagas Institute in late log stage were used. Parasites were maintained in
46 Schneider’s medium (Sigma-Aldrich Co., St. Louis, USA) supplemented with 10 % FBS, 50,000 IU/mL
47 penicillin and 50 µg/mL streptomycin.
48
49
50
51
52

53
54 BALB/c mice (male, 5-weeks old) were randomly divided in four groups of four animals per group.
55 Animals were inoculated at the base of the tail with 2 x 10⁷ promastigote forms of *L. (L.) amazonensis*
56 in stationary growth phase (final volume 25 µL), except for the healthy control group which was given
57 only physiological solution (25 µL). After 35 days of infection, treatment was started for 10 consecutive
58 days applied once daily. Animals were arranged as follows: group 1 was treated with AmB-TFs (0.5
59
60

1
2
3 mg/mL, 20 mg of formulation/day, topically applied), group 2 was treated with Glucantime® (50 mg/kg,
4 25 µL intralesionally injected), group 3 was the infected control group with no treatment and group 4
5 consisted on untreated and uninfected animals (healthy control group). Lesion size was monitored at
6 days 4, 21, 28, 31, 35, 42, 46, 51 and 56 post-infection. Skin parasitism was quantified 10 days after the
7 end of the treatment (at 56 days post-infection). The same animals were used to measure the lesion size
8 and the parasite load.
9
10
11

12
13 The parasitic load was quantified by limiting dilution analysis in fragments of the skin, at the point of
14 the parasite inoculation. Briefly, fragments of skin were collected and aseptically homogenized in
15 Schneider's medium. Skin suspensions were subjected to 12 serial dilutions with four replicate wells.
16 The number of viable parasites was determined based on the highest dilution that promastigotes could
17 grow after 10 days of incubation at 25 °C. *In vivo* experiments were repeated at least twice, and the
18 results were expressed by the arithmetic mean ± standard deviation. Statistical analyses were performed
19 using GraphPad Prism 5.0, and the nonparametric Mann-Whitney U test was used to evaluate the
20 differences between treated and infected control groups. Differences were considered statistically
21 significant at a 5 % significance level ($p < 0.05$).
22
23
24
25
26
27

28 **Topical pharmacokinetic studies**

29
30 CD-1 male mice (8 weeks old, 28 ± 2 g) were randomly split into two different groups ($n=3$) that
31 received topically AmB-TFs with or without the application of microneedles for 3 seconds (Derma Pen
32 with 12 metallic needles of 500 µm in length purchased from TBPHP, Ruboskizo, Madrid, Spain). Prior
33 to sample administration, hair was trimmed in the upper dorsal area of the body. A 1 cm² of internal
34 diameter plastic tube was adhered on the shaved area and 0.5 mL of AmB-TFs (0.86 mg mL^{-1}) was
35 applied. At different time points (0.5, 1, 2, 4 and 6 hours post-administration), animals were sacrificed
36 and subsequently, skin was removed and the area exposed to the formulation was cleaned with wet
37 cotton bud before storage at $-20 \text{ }^{\circ}\text{C}$ prior to AmB analysis.
38
39
40
41
42
43

44 Skin samples were analysed by tape-stripping. Thirty consecutive tape-strips of 1 cm² diameter (Punts®,
45 Etyprinter S.L., Barcelona, Spain) were adhered in the skin area where the formulation was deposited
46 under the application of a 100 g weight for 2 seconds. Strips were removed and individually introduced
47 into a plastic Eppendorf tube containing methanol (0.45 mL). Tubes were sonicated for 15 min at room
48 temperature and centrifuged (5,000 rpm for 5 min at room temperature). The supernatant was removed
49 and transferred to HPLC vials for further analysis using a validated method for AmB⁴⁸. After the
50 removal of the 30 layers, the remaining skin was weighted prior to being homogenised in a 1 mL of
51 PBS pH 7.4 using a mortar and pestle. Two extractions using methanol were performed (1 mL x 2).
52 After each extraction, the homogenate was vortexed (2 min) and centrifuged (8,000 rpm, 10 min) and
53 supernatant was collected and transferred into HPLC vials to be analysed as described above⁴⁸. One-
54
55
56
57
58
59
60

1
2
3 way ANOVA followed by a Tukey's post-hoc test was performed (Minitab® 16 software) and
4 differences were considered statistically significant at a 5 % significance level ($p < 0.05$).
5

6 7 **ASSOCIATED CONTENT**

8 9 **SUPPORTING INFORMATION**

10
11 The Supporting Information is available free of charge. Detailed methodology on the characterisation
12 of AmB transfersomes is provided (particle size, zeta-potential, encapsulation efficiency,
13 morphological studies) as well as detailed methodology regarding histology studies and an *in vitro*
14 antifungal efficacy, antiparasitic efficacy and macrophage cytotoxicity. Results regarding DOE studies
15 for AmB transfersomes (Figure S1-S7, Table S1 and S2) as well as *in vitro* antiparasitic efficacy and
16 macrophage cytotoxicity data (Table S3) are provided. Parasitic load measured in BALB/c mice treated
17 with various formulations are also summarised (Table S4).
18
19
20
21
22

23 **AUTHOR CONTRIBUTIONS**

24
25 Raquel Fernández-García^{1#}: Methodology (Formulation development, stability studies, morphology
26 studies, *in vitro* antifungal studies, haemolysis studies, *in vivo* pharmacokinetic studies), Formal
27 analysis, Investigation, Data Curation, Writing – Original Draft, Visualisation, Writing – Review &
28 Editing.
29

30
31
32 Larry Statts^{2#}: Methodology (Formulation development, DOE studies, Franz cells studies and histology
33 studies), Validation, Formal analysis, Investigation, Data Curation, Formal analysis, Writing – Original
34 Draft, Visualisation.
35

36
37
38 Jéssica A. de Jesus³: Methodology (*In vivo* efficacy studies), Validation, Formal analysis, Investigation,
39 Data Curation, Formal analysis, Writing – Original Draft.
40

41
42 M. Auxiliadora Dea-Ayuela⁴: Methodology (*In vitro* antileishmanial and macrophage cytotoxicity
43 studies), Validation, Formal analysis, Investigation, Data Curation, Formal analysis, Writing – Original
44 Draft.
45

46
47 Liliana Bautista²: Methodology (Formulation development and morphology studies), Formal analysis,
48 Investigation, Data Curation.
49

50
51 Rúben Simão¹: Methodology (*In vivo* pharmacokinetic studies), Formal analysis, Investigation.
52

53
54 Francisco Bolás-Fernández⁵: Supervision, Funding acquisition.
55

56
57 M. Paloma Ballesteros^{1,6}: Supervision, Review & Editing.
58

59
60 Marcia Dalastro Laurenti³: Resources, Data Curation, Writing – Original Draft, Supervision, Project
administration and execution, Funding acquisition

1
2
3 Luiz F. D. Passero^{7,8}: Methodology (*In vivo* efficacy studies), Validation, Formal analysis,
4 Investigation, Resources, Data Curation, Writing – Original Draft, Supervision, Project administration
5 and execution, Funding acquisition
6
7

8
9 Aikaterini Lalatsa^{2*}: Conceptualisation, Methodology (Formulation development, morphology studies
10 and histology studies), Validation, Formal analysis, Investigation, Resources, Data Analysis and
11 Curation, Writing – Original Draft, Visualisation, Supervision, Writing – Review & Editing, Project
12 administration and execution, Funding acquisition
13
14

15 Dolores R. Serrano^{1,6*}: Conceptualisation, Methodology (Formulation development, DOE studies,
16 Franz cells studies, *in vitro* antifungal efficacy, haemolysis studies, *in vivo* pharmacokinetic studies),
17 Validation, Formal analysis, Investigation, Resources, Data Curation, Writing – Original Draft,
18 Visualisation, Writing – Review & Editing, Supervision, Project administration and execution, Funding
19 acquisition
20
21
22
23

24 ACKNOWLEDGEMENTS

25
26 The authors are grateful to FAPESP (2016/0048-0) and HC-LIM50. Larry Statts was supported with an
27 Erasmus+ grant to undertake a placement at UCM, Madrid, Spain. This work was funded by an Ibero-
28 American Universities Union Research Collaboration Fund (Unión Iberoamericana de Universidades;
29 ENF03-2017) allowing student mobility exchange between UCM (Madrid, Spain) and USP (Sao Paulo,
30 Brazil).
31
32
33
34

35 CONFLICT OF INTERESTS

36
37 The authors declare no competing financial interest.
38

39 ABBREVIATIONS

40
41 AmB: Amphotericin B; AmB-TFs: Amphotericin B loaded transfersomes; DOE: Design of experiment
42 studies; DMSO: Dimethylsulfoxide; EE: Entrapment efficiency; HPLC: High performance liquid
43 chromatography; NaDC: Sodium deoxycholate; QbD: Quality by design; PBS: Phosphate buffered
44 saline; RBCs: Red blood cells; RH: Relative humidity; SC: Stratum corneum; TEM: Transmission
45 electron microscopy; TFs: Transfersomes
46
47
48
49

50 REFERENCES

- 51
52 1. Fernandez-Garcia, R.; de Pablo, E.; Ballesteros, M. P.; Serrano, D. R., Unmet clinical needs in
53 the treatment of systemic fungal infections: The role of amphotericin B and drug targeting. *Int J*
54 *Pharm* **2017**, *525* (1), 139-148.
55 2. Serrano, D. R.; Hernandez, L.; Fleire, L.; Gonzalez-Alvarez, I.; Montoya, A.; Ballesteros, M.
56 P.; Dea-Ayuela, M. A.; Miro, G.; Bolas-Fernandez, F.; Torrado, J. J., Hemolytic and pharmacokinetic
57 studies of liposomal and particulate amphotericin B formulations. *Int J Pharm* **2013**, *447* (1-2), 38-46.
58 3. Torrado, J. J.; Espada, R.; Ballesteros, M. P.; Torrado-Santiago, S., Amphotericin B
59 Formulations and Drug Targeting. *J Pharm Sci* **2008**, *97* (7), 2405-2425.
60

1
2
3
4
5
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

4. Jensen, G. M., The care and feeding of a commercial liposomal product: liposomal amphotericin B (AmBisome®). *J Liposome Res* **2017**, *27* (3), 173-179.
5. López, L.; Vélez, I.; Asela, C.; Cruz, C.; Alves, F.; Robledo, S.; Arana, B., A phase II study to evaluate the safety and efficacy of topical 3% amphotericin B cream (Anfoleish) for the treatment of uncomplicated cutaneous leishmaniasis in Colombia. *PLOS Negl Trop Dis* **2018**, *12* (7), e0006653.
6. Ganeshpurkar, A.; Vaishya, P.; Jain, S.; Pandey, V.; Bansal, D.; Dubey, N., Delivery of Amphotericin B for Effective Treatment of Candida Albicans Induced Dermal Mycosis in Rats via Emulgel System: Formulation and Evaluation. *Indian J Dermatol* **2014**, *59* (4), 369-374.
7. Serrano, D. R.; Gallagher, K. H.; Healy, A. M., Emerging Nanonisation Technologies: Tailoring Crystalline Versus Amorphous Nanomaterials. *Curr Top Med Chem* **2015**, *15* (22), 2327-2340.
8. Fernández-García, R.; Lalatsa, A.; Statts, L.; Bolás-Fernández, F.; Ballesteros, M. P.; Serrano, D. R., Transferosomes as nanocarriers for drugs across the skin: Quality by design from lab to industrial scale. *Int J Pharm* **2020**, *573*, 118817.
9. Cevc, G.; Blume, G., Lipid vesicles penetrate into intact skin owing to the transdermal osmotic gradients and hydration force. *Biochim Biophys Acta* **1992**, *1104* (1), 226-232.
10. Rajan, R.; Jose, S.; Mukund, V. P.; Vasudevan, D. T., Transferosomes - A vesicular transdermal delivery system for enhanced drug permeation. *J Adv Pharm Technol Res* **2011**, *2* (3), 138-143.
11. Singodia, D.; Gupta, G.; Verma, A.; Singh, V.; Shukla, P.; Misra, P.; Sundar, S.; Dube, A.; Mishra, P., Development and Performance Evaluation of Amphotericin B Transferosomes Against Resistant and Sensitive Clinical Isolates of Visceral Leishmaniasis. *J Biomed Nanotech* **2010**, *6*, 293-302.
12. Ruiz, H. K.; Serrano, D. R.; Dea-Ayuela, M. A.; Bilbao-Ramos, P. E.; Bolas-Fernandez, F.; Torrado, J. J.; Molero, G., New amphotericin B-gamma cyclodextrin formulation for topical use with synergistic activity against diverse fungal species and Leishmania spp. *Int J Pharm* **2014**, *473* (1-2), 148-157.
13. Silveira, F. T.; Lainson, R.; De Castro Gomes, C. M.; Laurenti, M. D.; Corbett, C. E. P., Immunopathogenic competences of Leishmania (V.) braziliensis and L. (L.) amazonensis in American cutaneous leishmaniasis. *Parasite Immunol* **2009**, *31* (8), 423-431.
14. Lalatsa, A.; Patel, P. V.; Sun, Y.; Kiun, C. C.; Karimi, F.; Zekonyte, J.; Emeriewen, K.; Saleh, G. M., Transcutaneous Anaesthetic Nano-enabled Hydrogels for Eyelid Surgery. *Int J Pharm* **2020**, 119003.
15. Kietzmann, M.; Lubach, D.; Heeren, H.J., The mouse epidermis as a model in skin pharmacology: influence of age and sex on epidermal metabolic reactions and their circadian rhythms. *Lab Animals* **1990**, *24* (4), 321-327.
16. Garnier, T.; Mäntylä, A.; Järvinen, T.; Lawrence, J.; Brown, M.; Croft, S., In vivo studies on the antileishmanial activity of buparvaquone and its prodrugs. *J Antimicrob Chemother* **2007**, *60* (4), 802-810.
17. Reddy, M. B.; Stinchcomb, A. L.; Guy, R. H.; Bunge, A. L., Determining Dermal Absorption Parameters in Vivo From Tape Strip Data. *Pharm Res* **2002**, *19* (3), 292-298.
18. Donnelly, R. F.; Singh, T. R.; Garland, M. J.; Migalska, K.; Majithiya, R.; McCrudden, C. M.; Kole, P. L.; Mahmood, T. M.; McCarthy, H. O.; Woolfson, A. D., Hydrogel-Forming Microneedle Arrays for Enhanced Transdermal Drug Delivery. *Adv Func Mater* **2012**, *22* (23), 4879-4890.
19. Kalluri, H.; Kolli, C. S.; Banga, A. K., Characterization of microchannels created by metal microneedles: formation and closure. *AAPS J* **2011**, *13* (3), 473-481.
20. Kim, Y. C.; Park, J. H.; Prausnitz, M. R., Microneedles for drug and vaccine delivery. *Adv Drug Deliv Rev* **2012**, *64* (14), 1547-1568.
21. Esfandiarpour, I.; Farajzadeh, S.; Rahnama, Z.; Fathabadi, E. A.; Heshmatkhan, A., Adverse effects of intralesional meglumine antimoniate and its influence on clinical laboratory parameters in the treatment of cutaneous leishmaniasis. *Int J Dermatol* **2012**, *51* (10), 1221-1225.

- 1
2
3
4
5
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60
22. Ben Salah, A.; Ben Messaoud, N.; Guedri, E.; Zaatour, A.; Ben Alaya, N.; Bettaieb, J.; Gharbi, A.; Belhadj Hamida, N.; Boukthir, A.; Chlif, S.; Abdelhamid, K.; El Ahmadi, Z.; Louzir, H.; Mokni, M.; Morizot, G.; Buffet, P.; Smith, P. L.; Kopydlowski, K. M.; Kreishman-Deitrick, M.; Smith, K. S.; Nielsen, C. J.; Ullman, D. R.; Norwood, J. A.; Thorne, G. D.; McCarthy, W. F.; Adams, R. C.; Rice, R. M.; Tang, D.; Berman, J.; Ransom, J.; Magill, A. J.; Grogl, M., Topical Paromomycin with or without Gentamicin for Cutaneous Leishmaniasis. *N Engl J Med* **2013**, *368* (6), 524-532.
23. Sosa, N.; Capitán, Z.; Nieto, J.; Nieto, M.; Calzada, J.; Paz, H.; Spadafora, C.; Kreishman-Deitrick, M.; Kopydlowski, K.; Ullman, D.; McCarthy, W. F.; Ransom, J.; Berman, J.; Scott, C.; Grogl, M., Randomized, double-blinded, phase 2 trial of WR 279,396 (paromomycin and gentamicin) for cutaneous leishmaniasis in Panama. *Am J Trop Med Hyg* **2013**, *89* (3), 557-563.
24. Kagan, L.; Gershkovich, P.; Wasan, K. M.; Mager, D. E., Physiologically based pharmacokinetic model of amphotericin B disposition in rats following administration of deoxycholate formulation (Fungizone®): pooled analysis of published data. *AAPS J* **2011**, *13* (2), 255-264.
25. Jiang, T.; Wang, T.; Li, T.; Ma, Y.; Shen, S.; He, B.; Mo, R., Enhanced Transdermal Drug Delivery by Transfersome-Embedded Oligopeptide Hydrogel for Topical Chemotherapy of Melanoma. *ACS Nano* **2018**, *12* (10), 9693-9701.
26. Jangdey, M. S.; Gupta, A.; Saraf, S.; Saraf, S., Development and optimization of apigenin-loaded transfersomal system for skin cancer delivery: in vitro evaluation. *Artif Cells Nanomed Biotechnol* **2017**, *45* (7), 1452-1462.
27. Morsi, N. M.; Aboelwafa, A. A.; Dawoud, M. H. S., Enhancement of the bioavailability of an antihypertensive drug by transdermal protransfersomal system: formulation and in vivo study. *J Liposome Res* **2017**, 1-12.
28. AEMPS AmBisome, data sheet. https://cima.aemps.es/cima/dochtml/ft/61117/FT_61117.html (accessed 29th December 2019).
29. Kaur, L.; Singh, K.; Paul, S.; Singh, S.; Singh, S.; Jain, S. K., A Mechanistic Study to Determine the Structural Similarities Between Artificial Membrane Strat-M™ and Biological Membranes and Its Application to Carry Out Skin Permeation Study of Amphotericin B Nanoformulations. *AAPS PharmSciTech* **2018**, *19* (4), 1606-1624.
30. Joshi, V.; Brewster, D.; Colanero, P., In vitro diffusion studies in transdermal research: A synthetic membrane model in place of human skin. *Drug Develop Deliv* **2012**, *12*, 40-42.
31. Uchida, T.; Kadhum, W. R.; Kanai, S.; Todo, H.; Oshizaka, T.; Sugibayashi, K., Prediction of skin permeation by chemical compounds using the artificial membrane, Strat-M™. *Eur J Pharm Sci* **2015**, *67*, 113-118.
32. Taylor, V. M.; Cedeño, D. L.; Muñoz, D. L.; Jones, M. A.; Lash, T. D.; Young, A. M.; Constantino, M. H.; Esposito, N.; Vélez, I. D.; Robledo, S. M., In vitro and in vivo studies of the utility of dimethyl and diethyl carbaporphyrin ketals in treatment of cutaneous leishmaniasis. *Antimicrob Agents Chemother* **2011**, *55* (10), 4755-4764.
33. Ryder, N. S.; Wagner, S.; Leitner, I., In vitro activities of terbinafine against cutaneous isolates of *Candida albicans* and other pathogenic yeasts. *Antimicrob Agents Chemother* **1998**, *42* (5), 1057-1061.
34. Morais-Teixeira, E.; Gallupo, M.; Rodrigues, L.; Rabello, A., In vitro interaction between paromomycin sulphate and four drugs with leishmanicidal activity against three New World *Leishmania* species. *J Antimicrob Chemother* **2014**, *69* (1), 150-154.
35. Hartsel, S.; Bolard, J., Amphotericin B: new life for an old drug. *Trends Pharmacol Sci* **1996**, *17* (12), 445-449.
36. Yardley, V.; Croft, S. L., A comparison of the activities of three amphotericin B lipid formulations against experimental visceral and cutaneous leishmaniasis. *Int J Antimicrob Ag* **2000**, *13* (4), 243-248.

1
2
3
4
5
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

37. Hong, Y.; Shaw, P. J.; Tattam, B. N.; Nath, C. E.; Earl, J. W.; Stephen, K. R.; McLachlan, A. J., Plasma protein distribution and its impact on pharmacokinetics of liposomal amphotericin B in paediatric patients with malignant diseases. *Eur J Clin Pharmacol* **2007**, *63* (2), 165-172.
38. Ordóñez-Gutiérrez, L.; Espada-Fernández, R.; Dea-Ayuela, M. A.; Torrado, J. J.; Bolás-Fernandez, F.; Alunda, J. M., In vitro effect of new formulations of amphotericin B on amastigote and promastigote forms of *Leishmania infantum*. *Int J Antimicrob Ag* **2007**, *30* (4), 325-329.
39. Dar, M.; McElroy, C.; Khan, M.; Satoskar, A.; Khan, G. M., Development and evaluation of novel miltefosine- polyphenol co-loaded second generation nano- transfersomes for the topical treatment of cutaneous leishmaniasis. *Expert Opin Drug Del* **2020**, *17* (1), 97-110.
40. González, K.; Diaz, R.; Ferreira, A. F.; García, V.; Paz, H.; Calzada, J. E.; Ruíz, M.; Laurenti, M.; Saldaña, A., Histopathological characteristics of cutaneous lesions caused by *Leishmania Viannia panamensis* in Panama. *Rev Inst Med Trop SP* **2018**, *60*:e8.
41. Gupta, J.; Gill, H. S.; Andrews, S. N.; Prausnitz, M. R., Kinetics of skin resealing after insertion of microneedles in human subjects. *J Control Rel* **2011**, *154* (2), 148-155.
42. Kalluri, H.; Kolli, C. S.; Banga, A. K., Characterization of Microchannels Created by Metal Microneedles: Formation and Closure. *AAPS J* **2011**, *13* (3), 473-481.
43. Van Bocxlaer, K.; Yardley, V.; Murdan, S.; Croft, S. L., Drug permeation and barrier damage in *Leishmania*-infected mouse skin. *J Antimicrob Chemother* **2016**, *71* (6), 1578-85.
44. Ekanayake-Mudiyanselage, S.; Aschauer, H.; Schmook, F. P.; Jensen, J. M.; Meingassner, J. G.; Proksch, E., Expression of epidermal keratins and the cornified envelope protein involucrin is influenced by permeability barrier disruption. *J Invest Dermatol* **1998**, *111* (3), 517-23.
45. ShinEtsu Metolose, data sheet. <http://www.metolose.jp/en/pharmaceutical/metolose.html> (accessed 14th January 2020).
46. Rodrigues, C.; Khalil, N.; Mainardes, R., Determination of amphotericin B in PLA-PEG blend nanoparticles by HPLC-PDA. *Braz J Pharm Sci* **2014**, *50*, 859-868.
47. Serrano, D. R.; Walsh, D.; O'Connell, P.; Mugheirbi, N. A.; Worku, Z. A.; Bolas-Fernandez, F.; Galiana, C.; Dea-Ayuela, M. A.; Healy, A. M., Optimising the in vitro and in vivo performance of oral cocrystal formulations via spray coating. *Eur J Pharm Biopharm* **2018**, *124*, 13-27.
48. Espada, R.; Josa, J. M.; Valdespina, S.; Dea, M. A.; Ballesteros, M. P.; Alunda, J. M.; Torrado, J. J., HPLC assay for determination of amphotericin B in biological samples. *BMC* **2008**, *22* (4), 402-407.
49. Millipore, M. Strat-M membrane. <https://www.in-cosmetics.com/novadocuments/255210?v=636053819429970000> (accessed July 18, 2019).
50. Serrano, D. R.; Gordo, M. J.; Matji, A.; Gonzalez, S.; Lalatsa, A.; Torrado, J. J., Tuning the Transdermal Delivery of Hydroquinone upon Formulation with Novel Permeation Enhancers. *Pharmaceutics* **2019**, *11* (4), 167.
51. Lalatsa, A.; Emeriewen, K.; Protopsalti, V.; Skelton, G.; Saleh, G. M., Developing transcutaneous nanoenabled anaesthetics for eyelid surgery. *Brit J Ophthalmol* **2016**, *100* (6), 871-876.
52. Kaur, L.; Singh, K.; Paul, S.; Singh, S.; Singh, S.; Jain, S. K., A Mechanistic Study to Determine the Structural Similarities Between Artificial Membrane Strat-M and Biological Membranes and Its Application to Carry Out Skin Permeation Study of Amphotericin B Nanoformulations. *AAPS PharmSciTech* **2018**, *19* (4), 1606-1624.
53. Lalatsa, A.; Statts, L.; de Jesus, J.A.; Adewusi, O.; Dea-Ayuela, M.A.; Bolas-Fernandez, F.; Dalastra, M.; Domingues, L.F.; Serrano, D.R. Topical Buparvaquone Nano-enabled Hydrogels for Cutaneous Leishmaniasis *Int J Pharm* **2020**, 119734.
54. Evans, B. C.; Nelson, C. E.; Yu, S. S.; Beavers, K. R.; Kim, A. J.; Li, H.; Nelson, H. M.; Giorgio, T. D.; Duvall, C. L., Ex vivo red blood cell hemolysis assay for the evaluation of pH-responsive endosomolytic agents for cytosolic delivery of biomacromolecular drugs. *J Vis Exp* **2013**, (73), e50166.

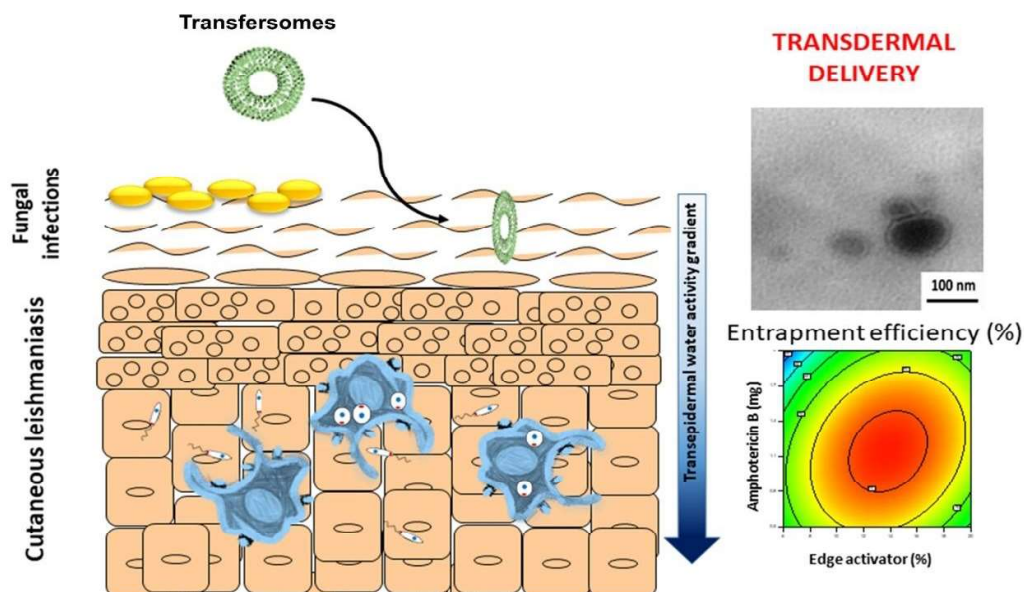
- 1
2
3
4 55. Dea-Ayuela, M. A.; Castillo, E.; Gonzalez-Alvarez, M.; Vega, C.; Rolon, M.; Bolas-
5 Fernandez, F.; Borrás, J.; Gonzalez-Rosende, M. E., In vivo and in vitro anti-leishmanial activities of 4-
6 nitro-N-pyrimidin- and N-pyrazin-2-ylbenzenesulfonamides, and N2-(4-nitrophenyl)-N1-
7 propylglycinamide. *Bioorg Med Chem* **2009**, *17* (21), 7449-7456.
8 56. Bilbao-Ramos, P.; Sifontes-Rodriguez, S.; Dea-Ayuela, M. A.; Bolas-Fernandez, F., A
9 fluorometric method for evaluation of pharmacological activity against intracellular Leishmania
10 amastigotes. *J Microbiol Methods* **2012**, *89* (1), 8-11.
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45

46 **For Table of Contents Use Only**
47
48

49 **Ultra-deformable lipid vesicles localise Amphotericin B in the dermis for the treatment of skin**
50 **infectious diseases**
51

52
53 Raquel Fernández-García^{1#}, Larry Statts^{2#}, Jéssica A. de Jesus³, Maria Auxiliadora Dea-Ayuela⁴,
54 Liliana Bautista², Rúben Simão¹, Francisco Bolás-Fernández⁵, Maria Paloma Ballesteros^{1,6}, Marcia
55 Dalastra Laurenti³, Luiz F. D. Passero^{7,8}, Aikaterini Lalatsa^{2*}, Dolores R. Serrano^{1,6*}.
56
57
58
59
60

1
2
3 Amphotericin B encapsulated within transfersomes enhances *in vitro* skin permeation resulting in
4 therapeutic levels after *in vivo* administration and a significant reduction in *Leishmania* parasites in
5 mice infected with cutaneous leishmaniasis. This formulation is readily translatable as a good
6 therapeutic alternative to current treatments for cutaneous leishmaniasis and fungal infections in
7 developed and developing countries.
8
9
10
11
12



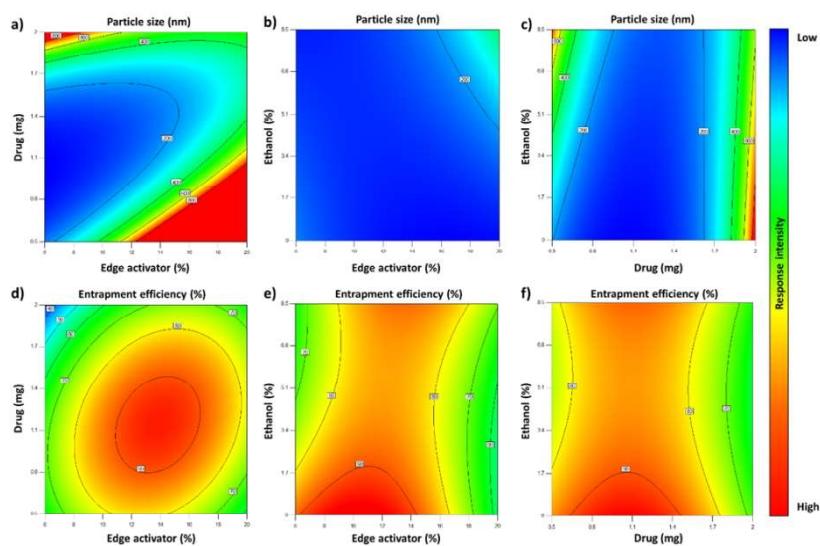


Figure 1: 2D Contour plots showing the effect of the amount of edge activator, drug and ethanol on particle size (a, b, c) and EE (d, e, f).

338x190mm (96 x 96 DPI)

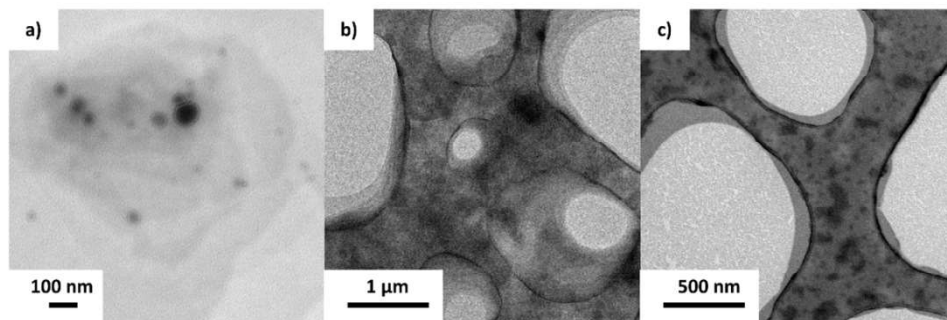


Figure 2: TEM micrographs of AmB-TFs; a) Freshly prepared AmB-TFs stained with 1 % uranyl acetate (Bar: 100 nm); b) Reconstituted freshly prepared freeze-dried AmB-TFs in deionised water stained with 2 % phosphotungstic acid (Bar: 1 μm); c) AmB-TFs after 28 days of storage at 4 °C stained with 2 % phosphotungstic acid (Bar: 500 nm).

338x190mm (96 x 96 DPI)

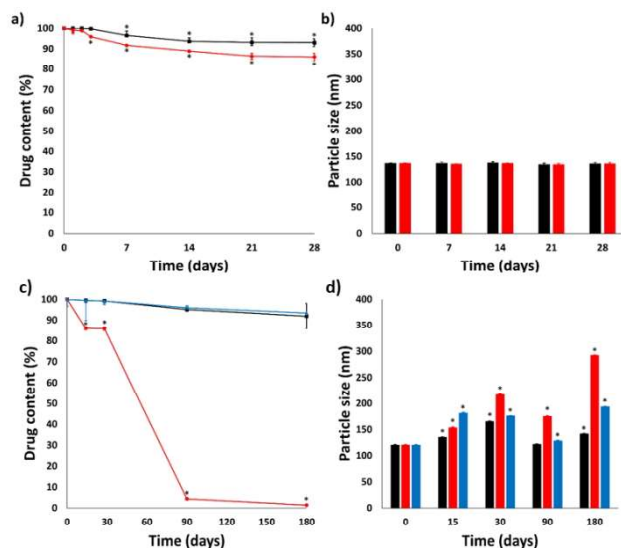


Figure 3: Physicochemical stability of liquid and freeze-dried AmB-TFs: a) Chemical stability of liquid AmB-TFs; b) Physical stability of liquid AmB-TFs. Key: 25 °C (red circles), 4 °C (black squares); * $p < 0.05$ is indicative of statistically significant difference between each time point and time 0 (one-way ANOVA post-hoc Dunnett's test). c) Chemical stability of freeze-dried AmB-TFs; d) Physical stability of freeze-dried AmB-TFs. Key: 25 °C, 10 % RH (black squares), 25 °C, 60 % RH (red circles), 4 °C, 10 % RH (blue triangles); * $p < 0.05$ is indicative of statistically significant difference between each time point and time 0 (one-way ANOVA post-hoc Dunnett's test).

338x190mm (96 x 96 DPI)

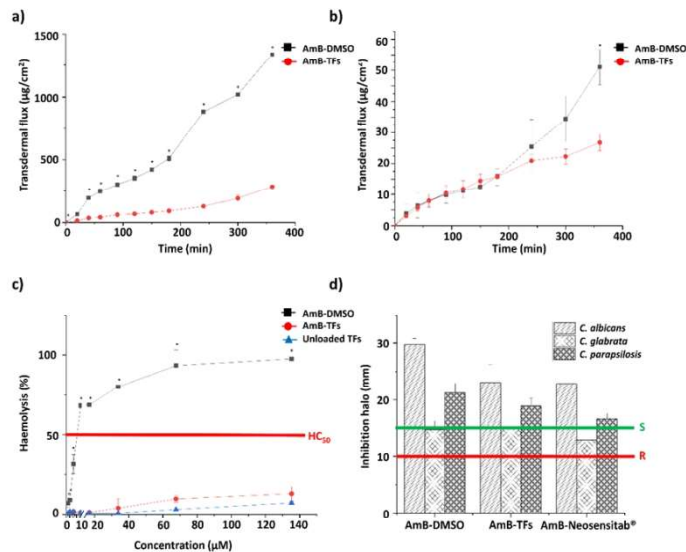


Figure 4: Permeability, toxicity and in vitro activity of AmB-TFs: a) Permeability of AmB-TFs and AmB-DMSO across Strat-M® membranes; b) Permeability of AmB-TFs and AmB-DMSO across mouse skin; c) Haemolytic toxicity of AmB-TFs, AmB-DMSO and unloaded TFs; d) Antifungal activity of AmB-TFs, AmB-DMSO and AmB-Neosensitabs®. Key: AmB-DMSO (black squares), AmB-TFs (red circles), unloaded TFs (blue triangles), concentration that produces 50 % of haemolysis (HC₅₀), sensitivity (S), resistance (R). Statistically significant difference is represented by * ($p < 0.05$) when comparing to AmB-DMSO with other formulations

338x190mm (96 x 96 DPI)

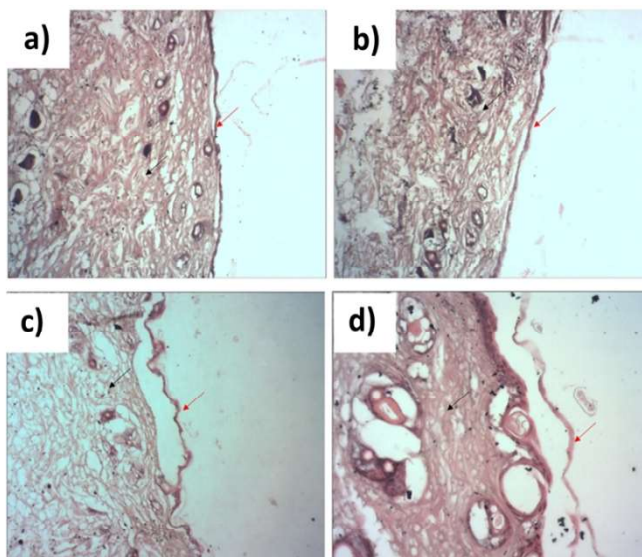


Figure 5: Micrographs of histological studies for treated skin with AmB -TFs and AmB dissolved in DMSO: a) mouse skin after exposure to AmB-TFs, 4x magnification; b) mouse skin after exposure to AmB-TFs, 10x magnification; c) mouse skin after exposure to AmB-DMSO, 4x magnification; d) mouse skin after exposure to AmB-DMSO; 10x magnification.

338x190mm (96 x 96 DPI)

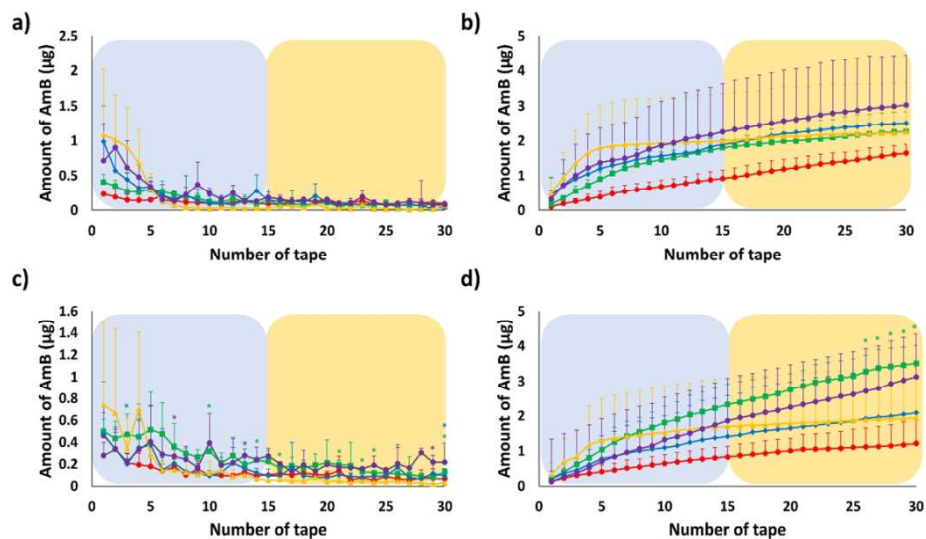


Figure 6: Averaged amount of AmB per tape strip (a, c) and cumulative amount of AmB (b, d) in mouse skin after 0.5, 1, 2, 4 and 6 h of post-administration without the application of microneedles (a, b) and after the utilization of microneedles (c, d). Key: 0.5 h (red circles), 1 h (green squares), 2 h (blue diamonds), 4 h (yellow triangles), 6 h (purple circles). The blue and orange panels represent the stratum corneum and the evaluated skin once the stratum corneum is removed, respectively. Statistically significant differences are represented by * ($p < 0.05$, one way-ANOVA post-hoc Tukey's test).

338x190mm (96 x 96 DPI)

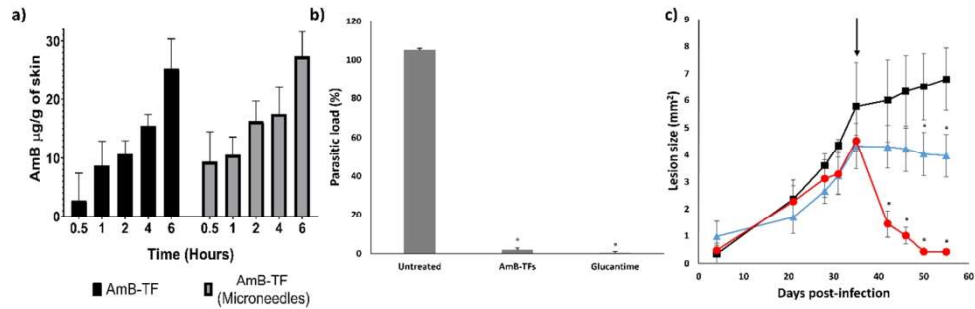


Figure 7. a) Amount of remaining AmB in the skin after removal of 30 tape-strips after the topical AmB-TFs administration (black bars) and topical AmB-TFs administration after application of microneedles (grey bars); b) In vivo antiparasitic activity (parasitic load) of AmB-TFs (0.5 mg/ml, 20 mg of formulation/day, once daily topically applied) and Glucantime® (50 mg/kg, once daily 25 µl intralesionally administered) in experimental cutaneous leishmaniasis caused by *L. (L.) amazonensis*; c) Evaluation of lesion size during the course of the infection. Key: untreated animals (black squares), AmB-TFs (blue triangles), Glucantime® (red circles). Arrow indicates the onset of treatment. Statistically significant differences between treated and untreated animals is represented by * ($p < 0.05$, Mann-Whitney U test).

338x190mm (300 x 300 DPI)